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State of the Art in Nanomedicine

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1.1 Intractable Diseases and Development of the Related Novel Therapy and Medicines

Lots of people get sick now and then in their lives, reducing their quality of life and even threatening their lives. Many diseases not only cause great suffering for people themselves but also for their families and then of the whole society, particularly for those intractable diseases, such as tumors or cancers, rheumatoid arthritis, cerebrovascular diseases (e.g. stroke, cerebral thrombosis, myocardial infarction), neural diseases (e.g. Parkinson's, Alzheimer's, depression), recurrent and infectious skin diseases (particularly relating to blood, endocrine, and immunity), and highly contagious and lethal infectious diseases (e.g. HIV, COVID-19), and so on. Among them, cerebrovascular diseases are the first killers of people, particularly for those more than 50 years old. There were about 1.79 million people in 2016 who died of these kinds of diseases all over the world, about 31% of global causes of death, according to the statistics of the World Health Organization (WHO). Cardiovascular outpatients in China are already more than 0.29 billion (B). Nearly three million people die from cardiovascular and cerebrovascular diseases in China every year, about 51% of the whole causes of death. Cerebrovascular diseases are the fifth cause of death in 2016, with about 373 deaths per 1 M people. In addition, these kinds of diseases preserve features of high suddenness, high disability rate (about 75% of the surviving patients have varying degrees of loss of labor ability and 40% are severely disabled), high recurrence rate, and more multiple complications (e.g. coronary heart disease, myocardial infarct, vascular dementia, subarachnoid hemorrhage, respiratory tract infection, and sudden deafness). China has entered an aging society like other developed countries (e.g. Japan) even though China is still a developing

country. The population of coronary artery disease (CAD) in China has increased from 2.27 M in 2016 to 2.53 M in 2020, with a compound annual growth rate of 2.7%. It was said that China's precision percutaneous coronary artery therapy (PCI) market has increased from ~\$25.7 M in 2016 to ~101.4 M in 2020, with a compound annual growth rate of ~ 40.8%. The global market scale of PCI also shows a growth trend, which was \$9.49 B in 2019 and was expected about \$13.26 B in 2025 with a compound annual growth rate of ~ 5.4% (<https://www.163.com/dy/article/HPGQBS2-R051481OF.html>; https://wenku.baidu.com/view/933bb2d7f624ccbff121dd36a32d7375a417c6c4.html?_wks_=_1711608332102&bdQuery=2023%E7%BB%8F%E7%9A%AE%E5%86%A0%E7%8A%B6%E5%8A%A8%E8%84%89%E6%B2%BB%E7%96%97%E5%85%A8%E7%90%83%E5%B8%82%E5%9C%BA%E8%A7%84%E6%A8%A1)).

Although cancers are the second killers of people, next to cerebrovascular diseases, the pain and burden of patients caused by cancers far outweigh the former due to their characteristics of chronic redundant diseases. It is said that there were about 19.29 M new cases of cancers, among which there were 10.06 M male cases and 9.23 M female cases according to the statistics in 2020. There were about 9.96 M death cases, including 5.53 M male cases and 4.43 M female cases. It is expected that there will be more than 21 M new cases in 2030 [1–3]. There are about 4.82 M and 2.37 M new cases of cancers, and about 3.21 M and 0.64 death cases of cancers, in China and the United States, respectively [1]. Partially thanks to innovative drugs and therapies promoted by medical technology, the overall trend of death cases of cancers in the United States is accelerated down since 1991 [1]. It is predicted that the new cases and death cases in 2023 will be continuously reduced by 410 K and 30 K compared with those in 2022. However, in China, the new cases and death cases of cancers in 2022 increased by 250 K and 210 K compared with those two years earlier (2020), and the 2022 death/new incidence rate in China is far more than that in United States (67% versus 27%) [1]. The death cases of lung cancers is the first among all death cases in China, and then the summed death cases of liver and pancreatic cancers. Particularly, the cases of liver cancers in China are almost half of the cases in the world. For many cases, cancers were found to be mostly the terminal stage [4–6]. While, thanks to vigorous anti-smoking measures in the United States, the first death case is breast cancer, not lung cancer, in the United States. The survival rates for some special cancers in China are lower than those in the United States, particularly for breast cancers and colorectal cancers. It is also said that cancer prognosis in China is much worse than that in the United States. China needs to make more efforts to provide effective cancer treatment and improve universal health coverage. New medicine and therapy of high anti-cancer efficiency are extremely urgent currently, especially for China. At the same time, the global market of anti-tumor medicine has increased to \$192.2 B in 2022 with a compound annual growth rate of ~12.7% while in China, the sales of anti-tumor drugs have been showing a steady growth trend in recent years. The market size of anti-tumor drugs reached \$28.2 B in 2020 and will have an estimated compound annual growth rate of ~16.1% from 2020 to 2025.

As for hyperuricemia and gout, there were about 1.03 billion (B) outpatients all over the world and about 0.18 B in China in 2022. The global market for gout

medicine was about \$3.0 B. The gout medicine market in China will grow rapidly in the future, which is expected to be about \$1.54 B in 2030. China has been known as the country with the largest population of diabetes in the world. The total number of people related to diabetes exceeded 260 million in 2018, including 114.39 M diabetes outpatients and 148.70 M pre-diabetes population. It is forecasted that the number of diabetes people will reach 320 M, which will create a huge market for diabetes medicine, with a potential scale expected to reach \$19.3 B.

There are four types of neural diseases: absence of symptoms, release of symptoms, irritation and shock, such as Parkinson's, Alzheimer's, Depression, and Huntington's diseases. There are more than 0.1 B people more than 15 years old with various mental disorders in China, among which there are about 16 M patients with severe mental disorders and most of the rest are people with mental or behavioral disorders such as depression or autism. These kinds of illnesses not only torture patients but also haunt their families for a long time. Particularly, they preserve some certain psychological infectivity (e.g. resulting in mass suicide groups), leading to great social harm. Developing these kinds of drugs for anti-mental disorders has to overcome the obstacle of passing the blood-brain barrier (BBB). It is more difficult for these drugs into nerve cells to break through the protective membranes of dendrites, myelin sheaths, axons, terminals, etc.

Clearly, fighting these intractable diseases is a long and arduous task for human beings, whose key is to develop diagnosis methods for early disease identification, innovative drugs, and subversive therapies. Starting from this century, medicine and health care entered into a rapid transformation period promoted by the interdisciplinary crossover of life science, biology, biophysics, biochemistry, nanotechnology, and information technology [7, 8]. As a result, many creative medicine or medical technologies sprout recently, such as personalized medicine, precise medicine, nanomedicine, and lots of innovative therapies, such as gene therapy (e.g. mRNA, DNA), targeting therapy (e.g. cell targeting, tumor microenvironment targeting), immunotherapy (e.g. PD1, PD-L1, vaccine, CAR-T), new physical field ablation therapy (e.g. nanosecond pulsed electrical field (nsPEF) ablation), new physicochemical therapy (e.g. ferroptosis, cuproptosis, photothermal therapy, photodynamic therapy, magnetothermal therapy, magnetodynamic therapy), and heavy particle radiation therapy (e.g. proton beam radiation, neutron scattering radiation, boron neutron capture therapy) [7–21].

Particularly, nanomedicines, which are translated from some functional nanomaterials, deal with nanoscale matters that can be used in biomedicine or biomedical engineering as bioprobes for the detection of biomolecule, organelle, cells or tissues, or as biosensors for the diseases or pathological metabolism diagnosis, or special drugs for some disease treatment or life function regulation. Based on nanodrugs and nanomedical engineering, lots of disruptive solutions have been advanced for the treatment of intractable diseases, such as anti-tumor nanomedicines [22], nanodrugs for rheumatoid arthritis [23], efficient nanodrugs for nerve or brain diseases by overcoming brain-blood barriers [10, 24], and oral administration nanodrugs for anti-HIV at low dosage [25]. Why does nanomedicine have so many special and powerful functions in disease diagnosis and therapy?

1.2 Key Features of Nanomedicines

There are several critical features of nanomaterials for their translation into special and efficient drugs and therapies. First, as shown in Figure 1.1a,b, most nutrition molecules and key functional molecules in the cell microenvironment range from molecule size to nanoscale (e.g. H_2O , glucose, phospholipid, protein, antibody, antigen, DNA, RNA). The cross-membrane transportation sizes for small molecules are usually less than 10 nm, which are better if less than 6 nm, and the best ones for each component are 2–3 nm or less (Figure 1.1a, the red dotted circle) [26]. Nanoscale materials can be controlled and synthesized by matching to the nanoscale range of the key biological macromolecules (e.g. protein transport pathways, lysosome, centriole, ribosome) very well. Once their surfaces are modified similarly to those biomolecules (e.g. full of $-OH$ ligands, amino acid side groups, glucose, lipids), they can preserve invisibility to the immune system and behave like zymogen during transportation. Second, sizes of organelles and majority of microstructures formed in cell membranes and organelles usually range from 30 nm (e.g. ribosome) to 10 μm (Figure 1.1a, the dotted pink circle, Figure 1.1c). Except that the nonmembrane structured ribosomes are 15–30 nm, the other organelles are generally ranging from 100 nm to 1.0 μm of mitochondria (the pink dotted circle in Figure 1.1a). As for the cells or bacteria for the motion space of nanomaterials and organelles, their sizes range from more than 1 μm for common bacterial to the smaller cells (i.e. red blood cells), and then at most up to less than 1 mm for the human eggs or frog cells (Figure 1.1a, the green dashed circle). The sizes for endocytosis and exocytosis for macromolecules, such as varieties of RNA, DNA, or proteins, range from several nanometers to several hundreds of nanometers or larger [27–29]. Three kinds of membrane transporting channels (i.e. voltage gates, ligand gates, and pressure activation channels) are all in the nanoscale [28, 29]. These size features of organelles and microstructures of cells provide enough free motion space for nanomaterials less than 10 nm and/or their aggregates less than 1.0 μm to exert their functions. As these nanomaterials are less than 10 nm, they can be surface-modified and functionalized easily by conjugating to some biomolecules and organelles, which facilitates their cross-membrane transportation and interaction with some certain organelles, and then targeting certain fine microstructures of organelles. Even they aggregate to several 10 nm or several 100 nm after biomolecule functionalization due to the strong interaction (e.g. coupling, crosslinking, salt bridges) or weak molecule interaction (e.g. van der Waals forces, hydrogen bonds), they can cross-membrane via endocytosis and exocytosis out or into cells and then lysis into nanometer or sub-nanometer effective components by special biomolecules or other cell microenvironment parameters (e.g. lysosomes, pH). Since they can be constructed with much similar surface properties and microstructures as those biomaterials in organisms, they can successfully avoid most of attacks from immunogenicity or autoimmunity, which can last their retention in organisms, leading to their unique enhanced permeability and retention (EPR) effect together with their high permeability [30–32].

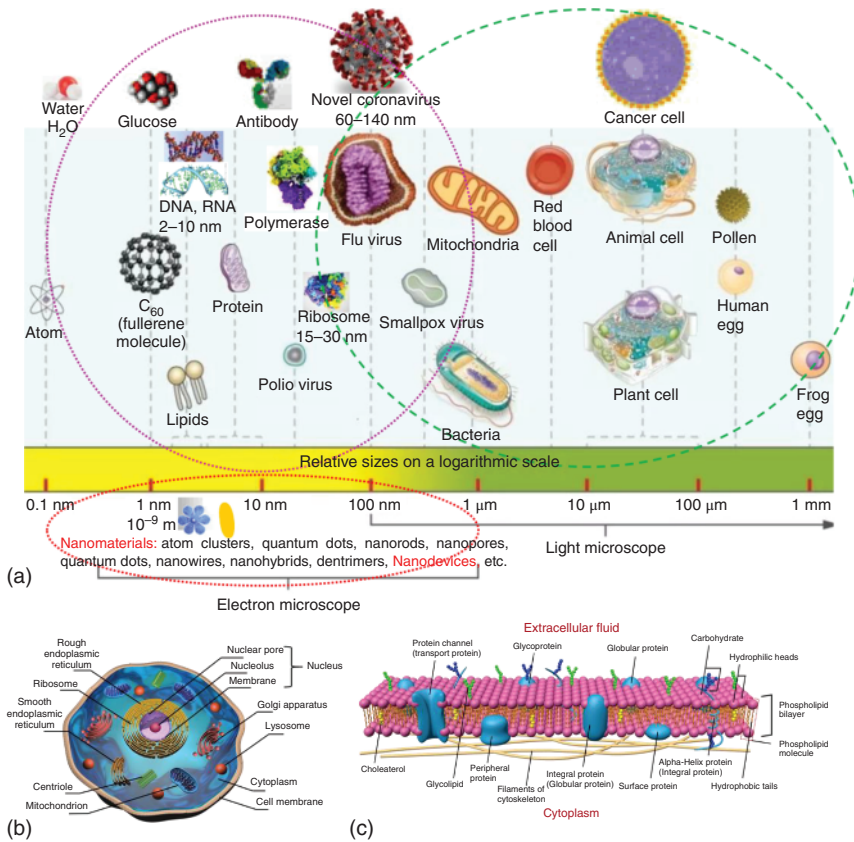


Figure 1.1 (a) Scale comparison of nanometer and some typical biomolecules and cells. Source: Adapted from Beijing Liuzhi Information Technology Co., Ltd./<http://www.360doc.com/showweb/0/0/1102300150/> last accessed December 28, 2023. The other small illustrations are original; (b) biomolecules and functional microstructures in cell membranes; and (c) organelles and microstructures in one single cell.

Clearly, due to their size effects and flexible surface modification and biomolecule functionalization, they show high biocompatibility and EPR effect as they interact with organs, tissues, cells, and organelles, which also benefit for them to overcome BBB for enhanced drug delivery to special focus in special organs or tissues and cells (e.g. brain or spinal, nerve cells, thrombus [preventing atherosclerosis]) [10, 33–35]. Particularly for those nanoparticles no more than 6 nm, better for 2–3 nm, they preserve much high bioactivity for efficiency-enhanced curative effect for treatment of tumors, cerebrovascular diseases, neural disease, etc. After they finish their bioactivity, they can be cleared via both urinary system and fecal system, which endows them high biosafety [10, 26, 36].

Nanomedicines can be constructed from organics, inorganics, or composites with single components or multi-hierarchy microstructures to realize some targeting functions: detection, and/or diagnosis, and/or therapy. Usually, their core parts can be ranged from 1.0 to 100 nm, which can be assembled into several hundreds

of nanometers or even into several micrometers. Broadly, those with nanometers or even micrometers by assembly of subnanometer components can be generally called nanomedicines. Recently, many multi-mode nanomedicines that preserve functions of detection, imaging, diagnosis, and therapy have been developed or called nanotheranostics and nanotherapeutics [8, 37, 38], which can be further developed as smart nanomedicine, or intelligent nanomedicine if some biomarkers for special molecules or cells are conjugated with these nanomedicines [39].

1.3 Nanotechnology Translational Nanomedicine: Emergence and Progress

Nanotechnology has developed rapidly over the past several decades and nanotechnology translational nanomedicine entered into a blowout development stage by coupling with other biomedical technology and artificial intelligence since 2015 [8, 10, 22, 27, 37, 40–58], as shown in Figure 1.2. Up to now, they have constructed many exciting contributions to the treatment of intractable diseases, such as cancers [7, 22, 114, 118], the rheumatoid arthritis [23], or the collagen-induced arthritis [107], nerve or brain diseases [10, 24], anti-HIV [25], cerebrovascular diseases [34, 42], and tissue regeneration (e.g. spinal cord regeneration [128]), skin diseases (e.g. diabetic wound healing) [129–133], as well as precise diagnosis of many special diseases and tracking some key biological processes as ultrasensitive visible bioprobes [83, 98, 134–149]. Figure 1.2 gives the historical timeline of major developments of nanomedicines, revealing a gradually developing process for nanoscale materials translational medicine since the first nanoscale medicine, or liposome nanostructures was published in 1964, which were constructed by phospholipids nanoemulsion used as drug carriers to encapsulate readymade low molecule medicine or drugs not compatible with body liquids [59, 114]. In 1964, silicon polymer of high biocompatibility was also developed into nanocarriers for prolonged drug lasting time [70]. The first organic nanodrug entering the technical level was Gris (Griseofulvin)-PEG (polyethylene glycol) oral tablet contenting sub-micro griseofulvin particles with ultra-high absorption rate, which was applied and issued in 1970 [150]. Langer and Folkman reported the first polymer nano-system for sustained controlled release of ionic molecules and macromolecules in 1976 [60]. In 1986, the EPR effect of nanoparticles was revealed, which is a unique vascular phenomenon for selective concentration of nanoscale agents in tumor or lesion tissues and can greatly increase the utilization efficiency of drugs [32, 61, 62]. For this goal, drugs with long retention time during circulation was desired. However, some negative effects during the drug circulation, such as destruction of immune response and cellular microenvironment factors (e.g. phagocytosis of macrophages, protein corona), have to be addressed by surface modification and using materials of high biocompatibility, hydrophilicity, and biodegradability [118, 151–153]. Therefore, long-circulating poly(lactic acid)-co-poly(ethylene glycol) (PLGA-PEG) copolymers-based drugs (e.g. PLGA-PEG encapsulating RNAi or genes) were developed in 1994 by Langer et al. since PLGA-PEG copolymers



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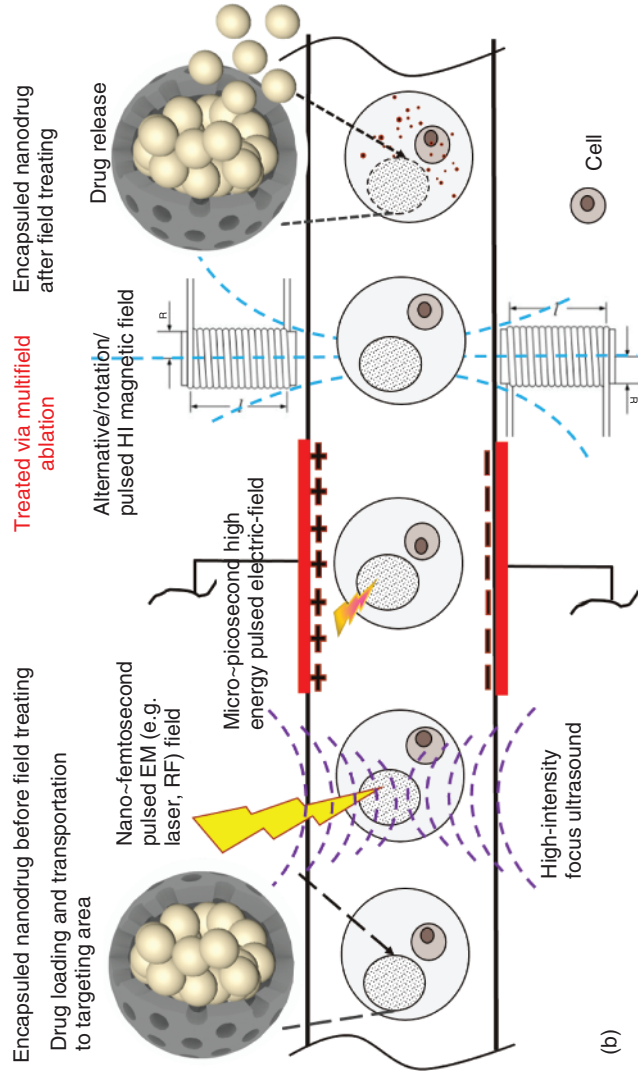


Figure 1.2 (continued). (b) The magnified scheme showing nanomedicine mediated multi-physical field (e.g. nanosecond–femtosecond electromagnetic (EM) field, high-intensity focus ultrasound (HIFU), microsecond–picosecond high-energy pulsed electric field, alternative/rotation/pulsed high-intensity magnetic field) ablation on single cells with controlled release and multi-modal therapeutical effects.

are of high biocompatibility and hydrophilicity [74]. However, active targeting is correspondingly of much importance when the tissue accumulation of drugs does not depend on EPR [154] or when the delivery of therapeutic agents requires active transcytosis of physiological barriers such as the intestinal mucosa or the BBB [155–157]. Therefore, many studies focused on the development of active targeting drugs and then the concept of active nanoparticle targeting was introduced in the 1970s [71, 72]. In 1976, some synthesized nanodrugs with active targeting functions made their way into clinical trials [30]. The liposomal doxorubicin (Doxil) nanodrugs of active targeting tumors were approved by FDA in 1995, showing greatly enhanced efficiency in cancer treatment [63, 114]. This is encouraging for the field of cancer nanomedicine. Then NP albumin-bound paclitaxel (nab-paclitaxel; Abraxane) became the second class of nanomedicines for long circulation to be approved by FDA in 2005 [63, 114] and commercialized, such as polymeric micelle paclitaxel (Genexol-PM) was successfully marketed in Korea in 2007 [158]. The nab platform enables formulation of hydrophobic drugs while largely mitigating the need to use toxic excipients, and then the regulatory filing for the approval of Vyxeos was projected in late 2016 [114]. Encouraged by the successful commercialization of Abraxane by addressing the enhanced retention time of drugs by the nanoscale strategy, the first targeted siRNA polymeric NPs (CALAA-01) were approved and entered into clinical trials in 2008 [50, 159]. Up to now, there are many targeting nanodrugs developed with controlled release including typical examples of targeted liposomes (for example, HER2) and single-chain variable fragment (scFv)-targeted liposome (MM-302) [160], the first targeted and controlled-release polymeric NP (BIND-014) [161], and the first targeted siRNA NPs (CALAA01) [50, 114, 162]. Simultaneously, the inorganic nanodrugs contenting 15 nm iron oxide particles were also approved as specific drugs for treatment of anemia in 1974 by FDA, following which many inorganic nanodrugs contenting gold, silver, iron oxides, silicon oxides, and titanium oxide nanoparticles have been gradually approved for clinical study by FDA [26, 114].

Besides the enhanced circulation time in body, the design and synthesis of nanodrugs have to consider how to avoid the immune response before they can be transported into the targeted lesion or cells. Many strategies were invented including the previous methods using materials of high biocompatibility, hydrophilicity, and biodegradability [118, 151]. Based on the direct bionics, cell membrane-coated NPs were further developed to construct cell membrane cloaking nanodrug aggregates by loading nanomedicine into the void cells (e.g. red blood cell) [79, 163, 164]. These cell membrane-coating nanodrug systems can efficiently evade immune response since surface characteristics of these cell membrane-coating nanodrugs are almost the same as those of healthy living cells [79, 163, 164]. During the development of nanodrugs, studies on EPR effects and the related biological mechanism of drugs continue to be paid attention to as their sizes are reduced to nanoscale. For these studies, many multi-mode nanobioprobes, such as protein biomarkers published in 2014 and the imaging agent of ferumoxytol in 2015, have been developed for predicting EPR effects and nanotherapeutic responses, which promotes the progress of nanodrugs with long retention time and active targeting. Together with the gradual realization

of multi-functions of nanodrugs, these studies finally led to the emergence of new fields of precise nanomedicine [8, 27], smart nanomedicine [40], and nanotheranostics [37, 42, 165]. According to the therapy effect analysis on nearly 350 kinds of new drugs, contenting nanomaterials submitted for FDA certification from 1970 to 2015 by FDA Drug Evaluation and Research Center in the United States (CDER), the application cases of nanodrugs increased gradually in the past 20 years, among which some have been used to serve people for the treatment of many intractable diseases (e.g. cancers, stroke, Parkinson's, Alzheimer's) [166].

With the progress of nanomedicine and their processing technologies (e.g. synthesis, structures and function characterization, multi-functionalization and clinical practice), the related biological mechanism on their fundamental biomedical effects has been deeply revealed, particularly the discovery of nonapoptotic forms of cell death of iron-based nanoparticles, termed as ferroptosis that can significantly promote death of tumor cells, by Dixon et al. [117]. Ferroptosis is dependent upon intracellular iron, but not other metals, and is morphologically, biochemically, and genetically distinct from apoptosis, necrosis, and autophagy. It has been confirmed that the small molecule ferrostatin-1 is a potent inhibitor of ferroptosis in cancer cells and glutamate-induced cell death in organotypic rat brain slices, suggesting similarities between these two processes like glutamate, erastin inhibits cystine uptake by the cystine/glutamate antiporter, creating a void in the antioxidant defenses of the cell and ultimately leading to iron-dependent, oxidative death. Thus, activation of ferroptosis results in the nonapoptotic destruction of certain cancer cells, whereas inhibition of this process may protect organisms from neurodegeneration for some neurodisease treatments [117]. Since 2016, a research frenzy on ferroptosis in tumor treatment was sparked and many transition metal-based medicines or nanomedicines have been found preserving similar nonapoptotic forms of cell death [94, 122, 167–169].

In 2022, the biological mechanism of copper-induced cell death was successfully revealed by Tsvetkov et al. [94]. Copper is an essential cofactor for all organisms, and yet it becomes toxic if concentrations exceed a threshold maintained by evolutionarily conserved homeostatic mechanisms. In human cells, copper-dependent, regulated cell death is distinct from known death mechanisms and is dependent on mitochondrial respiration. Tsvetkov et al. found that copper-dependent death occurred by means of direct binding of copper to lipoylated components of the tricarboxylic acid (TCA) cycle. This results in lipoylated protein aggregation and subsequent iron–sulfur cluster protein loss, which leads to proteotoxic stress and ultimately cell death. These findings may explain the need for ancient copper homeostatic mechanisms. Cell death is an essential, finely tuned process that is critical for the removal of damaged and superfluous cells. Multiple forms of programmed and nonprogrammed cell death have been identified, including apoptosis, ferroptosis, and necroptosis. Using genetically modified cells and a mouse model of a copper overload disorder, the researchers report that excess copper promotes the aggregation of lipoylated proteins and links mitochondrial metabolism to copper-dependent death. Lipoylation determines sensitivity to copper-induced cell

death. It can be proposed that Cu-based medicines preserve great promise in tumor cell treatment if they can be precisely targeted into the tumor cells.

With the investigation of the biomedical function of varieties of transition metal-based nanomedicines (e.g. Fe, Co, Cu, Au, Mn, and their compounds or alloys), their enzyme-like mechanism for disease treatment become more and more clear, which can catalyze many key molecule pathways (e.g. reactive ROS, glutamate) using nanomedicines based on the NPs of the transition metals, which can produce similar nonapoptotic forms of cell death in the cancer treatment as ferroptosis or cuproptosis [41, 94, 117, 170, 171], which can be reasonably termed as transition-metalloptosis [90]. Since almost all these nanomedicines preserve the enzyme-like catalyzing functions, which was further defined as a new research arena: nanoenzymes, recently [41, 58, 66, 95, 96, 104, 108–110, 172–175].

The research field of nanoenzymes has seen exponential growth over the past few years since the term was coined in 2016. This unique modality of cell death, driven by metal-dependent catalysis of some key biological reactions (e.g. ROS, glutamate, phospholipid peroxidation), is regulated by multiple cellular metabolic pathways, including produce of ROS; redox homeostasis; metal handling; mitochondrial activity; and metabolism of key amino acids, lipids, and sugars, in addition to various signaling pathways relevant to disease.

With the gradual reveal of the biomedical effects and their fundamental therapeutic mechanism, and the breakthrough in the controlled preparation methods and the administration technologies of nanomedicine, nanomedicine ushered in a blowout of development since 2016, as shown in Figure 1.2. Particularly, besides nanoenzyme functions [41, 58, 66, 95, 96, 104, 108–110, 172–175], many of them have played key roles in the overcome of multi-drug-resistant (MDR) during cancer treatment [176–180], in the development of innovative immunotherapy by the reveal of their immunological effects for nanoimmunotherapy [27, 37, 40, 47, 89, 110, 114, 118, 124, 168, 181–183].

MDR is a frequently encountered thorny issue as using traditional or even some innovative drugs to treat many diseases, particularly for some persistent infectious diseases and difficult miscellaneous diseases (e.g. cancers), which impedes the successful treatment of targeting diseases [176–180]. Developing novel long-circulating, self-assembled core-shell nanoscale coordination polymer (NCP) nanoparticles that efficiently deliver multiple therapeutics with different mechanisms of action to enhance synergistic therapeutic effects is an innovative strategy to overcome this multi-drug-resistant issue [179]. For example, Lin et al. invented NCPs code liver chemotherapeutics and siRNAs to eradicate tumors of cisplatin-resistant ovarian cancer in 2016 [178]. These NCP particles contain high payloads of chemotherapeutics cisplatin or cisplatin plus gemcitabine in the core and pooled siRNAs that target MDR genes in the shell. The NCP particles possess efficient endosomal escape via a novel carbon dioxide release mechanism without compromising the neutral surface charge required for long blood circulation and effectively downregulate MDR gene expression in vivo to enhance chemotherapeutic efficacy by several orders of magnitude. By silencing MDR genes in tumors,

self-assembled core-shell nanoparticles suggest a more effective chemotherapeutic treatment for many challenging cancers [178].

1.4 Interdisciplinary Features of Nanomedicines: Multi-mode and Multi-function Features Promoting Nanomedicine-mediated Immunotherapy and/or Physical Field Ablation Therapy for Subversive Therapy

Tumor immunotherapy has become one of the key innovative methods in tumor treatment and many immunotherapy drugs (e.g. PD-1, PD-L1, CTLA-4) and therapy. (e.g. cart-T) have been developed recently. However, existing cancer immunotherapy drugs work in only 20%–30% of patients [44, 73], particularly for those patients with solid tumor. In some cases, even when the checkpoint molecules are blocked, there are too few active T cells around to sound the immune alarm, says Jedd Wolchok, a cancer immunotherapy expert at the Memorial Sloan Kettering Cancer Center in New York City [73]. Additionally, the key reason is that tumors do not display enough of the T cell's targets, so-called tumor antigens, on their surface. However, nanoparticles and their functionalized species can behave similar to antigens as they enter into bodies [44, 73, 184]. The immunological mechanism of nanomedicine has been studied intensively for the treatment of tumors in the past decade. Results indicate that nanomedicines preserve intensive immune abscopal effects and have great potential as artificial antigens to activate and train immune cells [185], and they can even reprogram cancer cells or immune cells to reshape the tumor immune microenvironment [37, 46–49, 51, 184, 186, 187]. It is said that tumor cells are usually produced every day in our body due to a variety of causes, which will not lead to cancer if they can die through their routine apoptosis themselves or be cleaned by our immune system [47, 48, 113, 188–192]. However, tumor cells are smart and can escape from our immune system since they can disguise themselves by releasing some signals or chemicals to let immune cells confirm that they are healthy cells, and then suppress the secretion function of immune cells not to release the corresponding cytokines killing cancer cells [47, 48, 54, 113, 189, 190, 193]. The immunological abscopal effect of nanomedicines was revealed in 2017 by Min et al. [49]. One function of nanomedicines on the immune system is to activate or awaken immune cells, called an immune agonist [44, 73, 178, 194], such as using the paclitaxel nanoparticles to awaken immune system to fight against cancer studied by Tang et al. [194]. In 2016, Lin et al. developed self-assembled core-shell NCP nanoparticles that efficiently delivered multiple therapeutics with different mechanisms of action to enhance synergistic therapeutic effects for ovarian cancer treatment [44]. These NCP NPs contained high payloads of chemotherapeutics cisplatin or cisplatin plus gemcitabine in the core and pooled siRNAs that target multi-drug-resistant (MDR) genes in the shell [44].

Some physical therapies, such as radiation therapy [44, 73] and electrical field therapy [13–15, 195, 196], can break tumor cells to expose some antigens. Therefore, the self-immune systems of some patients can be activated to produce

immune response effects similar to immunotherapy after some physical therapy [15, 44, 178, 197, 198]. Based on this phenomenon, Lin et al. from the University of Chicago invented photosensitive ultra-small nanodrugs for tumor treatment, which can ignite the immune responses for some tumors insensitive to immunotherapy by coupling them with radiation therapy [44, 73]. The recent progress suggests that these nanodrug-mediating immunotherapies and/or physical field treatments are expected to enter into clinical trials, which have become the best partner in the field of immunotherapy [15, 37, 44, 73, 178, 197–199].

Another immunological function of nanomedicines was to reprogram immune cells to recognize cancer cells advanced in 2018 by Roth et al. [115] and Yang et al. [200], such as reprogramming the function and specificity of human T cells with nonviral genome targeting for anti-cancer therapy [115]. This strategy has been modified for the development of Parkinson's disease therapy using nanoparticles, such as electromagnetized gold nanoparticles mediating direct lineage reprogramming into induced dopamine neurons for the treatment of Parkinson's [10].

At the same time, some artificial antibodies (vaccines) have been developing, with active targeting functions [46]. In 2018, Cao and Wang developed a conformational engineering method to create an NP-based artificial antibody, denoted “Goldbody,” through conformational reconstruction of the complementary-determining regions (CDRs) of natural antibodies on gold NPs (AuNPs) [46]. Upon anchoring both terminals of the free CDR loops on AuNPs, the “active” conformation of the CDR loops can be reconstructed by tuning the span between the two terminals, endowing these inorganic NPs the original specificity. Two Goldbodies have been created by this strategy to specifically bind with hen egg white lysozyme and epidermal growth factor receptor, with apparent affinities several orders of magnitude stronger than that of the original natural antibodies. As a result, it is possible to create protein-like functions on these much more stable metallic NPs in a protein-like way, namely by tuning flexible surface groups to the correct conformation, which will finally build up a category of Goldbodies that can target different antigens and thus be used as substitute for natural antibodies in various applications [46]. The first approved anti-body nanodrug Cabiliv (Caplacizumab-Yhdp) was approved by the European Union and then commercially launched for clinical use in 2018, which became the first nano anti-body drug for the treatment of allergic purpura (Henoch-Schonlein syndrome, HSS) in the world. (https://www.sohu.com/a/252250535_119250; <https://www.vodjk.com/news/180904/1503187.shtml>: Cabiliv™ [caplacizumab] approved in Europe for adults with acquired thrombotic thrombocytopenic purpura [aTTP]; Sanofi gets EU OK for Ablynx flagship drug Cabiliv). This drug was then approved by FDA in the United States in February 2019 (https://www.sohu.com/a/252250535_119250; <https://www.drugs.com/history/cablivi.html>). Since then, nanomedicines not only with more intimate to immunological effects but also with multiple-therapy functions and multi-targeting functions (e.g. cancer cells, organelles, or tumor microenvironment) have been developed forming a novel field of nano-immunotherapy up to now [47, 48, 51, 57, 101, 118, 182–184]. If readers need more details on the immunological effects of nanomedicines, Chapter 10 in this monograph can be referred to.

Simultaneously, coupling of nanomedicines to some advanced biophysical or biochemical methods for subversive combined therapies has been on the way for difficult miscellaneous diseases [27, 37, 40–42, 47, 58, 89, 110, 114, 118, 124, 165, 168, 181–183, 201–203]. Besides their biomedical functions (e.g. immunological effects, enzyme-like functions), nanomedicines constructed by nanohybrids conjugating to varieties of biochemical drugs or preparation, preserve unique physicochemical characteristics and can simultaneously interact with several physical fields (e.g. electrical field, magnetic field, optical field, ultrasound field, electric–magnetic field) [37, 46–48, 51, 186, 187]. Multi-mode therapy and diagnosis based on these multi-functional nanomedicine-mediated physical field ablation and/or the corresponding molecule imaging and bioprobe function have been developed recently into one novel medical methodology with both diagnosis and therapy functions, or nanotheranostics [37, 42]. Particularly, nanotheranostics as these multi-mode nanomedicines coupling with physical field ablation preserve greatly enhanced therapeutical effects and in situ precise diagnosis functions for treatment of varieties of intractable diseases by comparing with their counterparts (either physical field ablation or solely nanomedicine), many of which have been implemented in the clinical trial [37].

Besides the enhanced apparent therapeutic effect due to the synergistic effects among varieties of physical fields and nanomedicines, another amazing achievement of nanomedicine mediated physical field ablation in their biomedical application is the dramatically improved immunological effects that are far beyond that one single physical field or nanodrug can do. Table 1.1 summarizes the multi-mode of action, advantages and disadvantages, immunological effects, and clinical progress of multi-modal ablation by multiple physical field coupling.

Currently, there are five typical physical field coupling modes in the road of clinical trials as follows. (i) The coupling of high-intensity focused ultrasound (HIFU), with light irradiation (PR) or fluorescence excitation (CLE) produces dual mode and multi-modal therapeutic effects, such as tissue tearing, cell fragmentation, sonodynamic therapy (SDT), and photochemical kinetic ablation (PDT), leading to more active molecules (e.g. reactive oxygen species [ROS]) and high-temperature thermal effects [204–206]. These effects promote the release of tumor antigens to activate immune cells, induce inflammatory reactions, and enhance immune memory of related immune cells. To date, this kind of HIFU coupling to PP or CLE technology is still in preclinical stage. (ii) The coupling of HIFU and electrical field (EFT) produces dual mode or multi-modal effects, such as tissue tearing and cell fragmentation caused by ultrasound, and electrochemical (EDT) or electrostatic field polarization (ESFP) by electrical fields, and pore formation and polarization by nsPEF for cell internalization of drugs and surface electrical dipole regulation of sub-cellular structures [207], leading to ROS formation, reversible perforation, and electrical dipole interaction with organelles at the related microregions or biomolecules and their functional groups [208]. This kind of combined therapy by coupling HIFU and EFT preserves multi-immunological effects, such as immune cell activation, enhanced anti-tumor immune response, immune related gene expression regulation (pro-inflammatory and anti-inflammatory factors),

Table 1.1 Working modes of the currently developed multi-modal ablation therapy based on multi-physics coupling and their main features and key challenges, immunological effects, clinical progress, and main affiliation.

Modes of multi-physical field coupling		Energy/Momentum mode and/or biochemical reaction activation		Multi-functional modes at work		Main features	Key challenges	Immunological effects and mechanisms	Affiliation (company or institute)	Clinical stage	References
High-intensity focused ultrasound (HIFU), light irradiation (PR)/fluorescence excitation (CL); dual mode multi-modal		Tissue tearing, cell fragmentation, sonochemical therapy (SDT), photochemical kinetic ablation (PDT)		Reactive oxygen species (ROS), high-temperature thermal effects		High tissue penetration, spatiotemporal control, and synergistic effects	Cause thermal damage to people	Promote the release of tumor antigens, activate immune cells, induce inflammatory reactions, and enhance immune memory	Ruiya biotechnology, Canada Covidien, United States	Preclinical	[204–206]
High-intensity focused ultrasound (HIFU) plus electrical field (EFT); dual mode multi-modal		Tissue tearing and cell fragmentation caused by ultrasound, electrochemical (EDT) or electrostatic field polarization, nanosecond pulsed electric field (nsPEF) pore formation and polarization		ROS, reversible perforation, and interaction with organelles or biomolecular microregions and functional groups		High tissue penetration, oxygen independence, and synergistic effects	Thermal damage to human body, embedded electrode	Immune cell activation, enhanced anti-tumor immune response, immune related gene expression regulation (pro-inflammatory and anti-inflammatory factors), angiogenesis inhibition, and immunosuppressive cell regulation	MIT and SonaCare Medical Co, Shenzhen Maiwei Medical Company, University of Science and Technology Beijing	Preclinical, Clinical Phase I, II	[207, 208]

(Continued)

Table 1.1 (Continued)

Energy/Momentum mode and/or biochemical reaction activation		Multi-functional modes at work	Main features	Key challenges	Immunological effects and mechanisms	Affiliation (company or institute)	Clinical stage	References
Modes of multi-physical field coupling	mode (modality)							
Photoenergy irradiation (PR)/ chemical fluorescence excitation (CLE) plus electric field (EFT): dual mode multi-modal	Photodynamic therapy (PDT), electrochemical therapy (EDT), or electrostatic field polarization	ROS, high-temperature thermal effects, etc.	Temporal and spatial control, oxygen independence, and synergistic effects	Thermal damage to human body, embedded electrode	Activation and proliferation of immune cells and immune regulatory cells, enhancement of anti-tumor immune response and expression of immune related factors (pro-inflammatory and anti-inflammatory)	Griffin Adam holiday, Norway Photocure ASA, Hangzhou Ruidi Biotechnology Co., Ltd	Preclinical	[209, 210]
Electromagnetic field/magnetic field plus temperature field ablation: dual/triple mode multi-mode	Radiofrequency ablation (RFA)/ alternating magnetic field heat plus cryoablation (CryoA) cold plus radiofrequency chemical dynamic ablation	High temperature thermal effect, low temperature freezing effect, cell rupture	High tissue penetration, targeted therapy, noninvasive, synergistic effects	Depth limitation, uneven heat distribution, damage to people	Immune cell activation and enhancement (tumor-specific T cells and NK cells), anti-tumor immune response enhancement, immune-related gene expression regulation, immune regulatory cell regulation	Medtronic, United States; Immodulon Therapeutics Ltd, United Kingdom; Shanghai Meijie Medical Technology Co., Ltd.; Beijing Haijeya Medical Device Co., Ltd, Magforce AG, Germany; Lodespin Labs, Canada	Preclinical, Clinical Phase I, II	[211–214]

Electrical field plus radio-frequency electromagnetic field plus plasma physics: dual/three-mode multi-mode	Radio frequency ablation (RFA) plus electro-chemical therapy (EDT) plus electrostatic field polarization or pulsed electric field (PEF) ablation, or plus low-temperature plasma (CAP)	ROS, thermal effect, alternating electrical or electrostatic field, and pulse electric field polarization and activation, plasma activation	Targeted therapy, synergistic effects, noninvasive, and low toxicity side effects	Improved accuracy, parameter and dose optimization, tumor type free	Stimulate the activation and proliferation of immune cells (natural killer cells [NK cells] and cytotoxic T lymphocytes [CTLs]), inflammatory response, tumor microenvironment regulation, and promote tumor antigen expression	Oncosec Medical Incorporated, Korea Adtec Healthcare	Preclinical, Clinical Phase I, II	[215]
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Source: Son et al. [217]/Royal Society of Chemistry.

angiogenesis inhibition and immunosuppressive cell regulation. Most of these therapies are in preclinical stage and some of them have been into clinical Phase I or II stage. (iii) The coupling of photo irradiation (PR) and/or chemical fluorescence excitation (CL) with EFT can also produce multi-modal therapeutic effects, such as photodynamic effect therapy (PDT) mode, electrochemical reaction therapy (EDT) mode and ESFP mode, which can ignite activation and proliferation of immune cells and immune regulatory cells, can enhance anti-tumor immune response and the related expression of immune-related factors (e.g. pro-inflammatory and anti-inflammatory) [209, 210]. This kind of multi-mode therapy is currently in pre-clinical stage. (iv) The coupling of EM field and/or magnetic field with temperature field ablation, which can produce the combination of dual or triple mode therapy, such as the combination of two or more ablation modes of radiofrequency ablation (RFA), alternating magnetic field heat, cryoablation (CryoA) cold ablation, and radiofrequency chemical dynamic ablation [211–214]. These multi-mode therapies can preserve the below immunological effects: immune cell activation and function enhancement (tumor-specific T cells and NK cells), enhanced anti-tumor immune response, and regulation of immune-related gene expression and immune regulatory cell. (v) The coupling of electrical field ablation, radiofrequency EM field ablation and plasma ablation, which can result in the multi-modal combination of RFA, EDT, ESFP, PEF, and low-temperature plasma (CAP). Studies on these multi-modal combinations indicate that they can activate the immune cells, stimulate the proliferation of immune cells (e.g. natural killer cells [NK cells] and cytotoxic T lymphocytes [CTLs]), promote tumor antigen expression, enhance the inflammatory response by recruiting more immune cells into lesions, and regulate the tumor microenvironment. Generally, most research suggests that multi-physical field coupling ablation can produce much more improved therapeutical effects, particularly in the activation of immune cells, enhancement of immune responses and the regulation of immune system, more than one single physical field mode due to their multi-field synergistic effects [215]. However, recent progress suggests that these immunological effects are generally not as great as desired when they are entering into the clinical trial stages, and most of these multi-modal therapies by the combination of different physical fields need agonists or multi-mode responsive nanomedicines to amplify their immunological effects and the final therapeutical effects or overcome some shortcomings [11, 37, 38, 42, 165, 207].

Typical cases of nanomedicines mediated physical-field ablation therapies were summarized in Table 1.2, which shows a brief description of their working modes, therapeutical effects, and anti-tumor applications. These multi-mode nanomedicines could also behave like agonists or amplifiers for their immunological effect by improving tri-interactions among medicines, physical fields, and lesions.

There are generally about nine types of multi-mode therapies based on nanomedicines mediated physical field ablation. (i) Nanomedicines (e.g. liposome nanodrugs) mediated HIFU by Indian Sun Pharmaceutical and Taiwan Toyo Pharmaceutical can result in tissue tearing and cell fragmentation by sonodynamic therapy (SDT) that increase the nanodrug cell internalization, utilization, and safety via overcoming BBB, which has entered into the clinical phases I and

Table 1.2 Working modes, therapeutical characteristics, applications, representative institutions, and clinical progress of nanomedicine-mediated physical field ablation therapies.

Physical ablation mode	Energy/Momentum or biochemical activity or working mode	Nano drug carrier	Conjugating drugs	Imaging mode	Therapeutical Application characteristics/fields	Representative institutions	Clinical stage	References
High-intensity focused ultrasound (HIFU)	Tissue tearing and cell fragmentation Sonochemical therapy (SDT)	Liposomes	Small molecules-macromolecules-nanomedicines	Ultrasonic	Enhances delivery safety and efficiency of drug utilization administration	Indian sun pharmaceutical	Phase I/II	[217–221]
					Triggers drug release	Taiwan Toyo Pharmaceutical	Phase I/II	[222–224]
					Greatly inhibiting tumor recurrence and preventing tumor metastasis	Soochow University; Macau University of Science and Technology	Phase I/II	[105]
Traditional electro-magnetic field	RF ablation (RFA)	Polymeric nanoparticle	Biomacromolecules	-	Blood brain barrier, etc.	The Fifth Medical Center of Chinese People's Liberation Army General Hospital	Preclinical	[102]
	RF-CDT				Liver cancer, ablation effect etc. and prevent recurrence			
Microwave ablation (MWT)	Microwave hyperthermia (MTT)	Liposomes	Small molecule drugs	-				
Microwave-dynamic (MDT)								

(Continued)

Table 1.2 (Continued)

Physical ablation mode	Energy/Momentum or biochemical activity or working mode					Nano drug carrier	Conjugating drugs	Imaging mode	Therapeutical characteristics	Application fields	Representative institutions	Clinical stage	References
New electro-magnetic field	Photo irradiation (PR) or CLE, pulsed laser photogenesis, photoshock	Photochemical photodynamic therapy (PDT)	Polymer, core-shell metal NPs	Macromolecular/small molecule drugs, porphyrins/saponins	Optical	Precision treatment	Breast cancer, liver cancer, etc.	Fudan	Clinical	[225–230]			
		Photothermal ablation (PTA)	Inorganic metal NPs	Iron oxide nanomedicine	MRI	The curative effect is clear, and combined with other ways to enhance its curative effect	Prostate cancer, glioblastoma, etc.	AMAG Pharmaceuticals; Advanced Magnetics, Inc	Phase I/II	[231–236]			
		Chemiluminescence biochemical reaction excitation (CL PDT)	Inorganic NPs, liposomes, etc.	Photosensitizers, – small molecule drugs	–	High tumor targeting and high efficiency	Lung cancer, etc.	Seoul National University; Shanghai Institute of Silicate, Chinese Academy of Sciences	Preclinical	[237–239]			
X ray		X-ray photochemical dynamics (PDT)	Inorganic metal nanoparticles	Sustained luminescent nanoparticles	–	Low dose X-ray can activate	Breast cancer	Memorial Sloan Kettering Cancer Center; Fuzhou University	Preclinical	[240, 241]			
		Radionuclide mediating photochemical dynamic therapy (CR PDT)	Polymers, inorganic NPs	Photosensitizer	–	Expanding the application scope of radiation therapy	Breast cancer, liver cancer, etc.	China Pharmaceutical University	Preclinical	[80, 237]			

High energy radiation therapy (HRT)	Isotope decay emits high energy metal NPs γ or β Isoray	Inorganic metal NPs	Au, Bi, Gd, Cs ¹³¹ complexes	MRI, CT, nuclear imaging	Enhance the curative effect of radiotherapy	Liver cancer, pancreatic cancer, esophageal cancer, nonsmall cell lung cancer, etc.	Johnson & Johnson's subsidiary Janssen Pharmaceuticals, nanobiotix, IsoRay company	Preclinical, Phase I/II	[238, 242–245]
Electrical field	Conventional electric field	Electrochemical (EDT) or electrostatic field polarization	Inorganic metal nanoparticles	Pt nanoparticles, – etc.	Minimal invasion and uniform ablation covering the relatively large tumors wholly	Breast cancer, etc.	Zhejiang University	Preclinical	[199]
		Millisecond to microsecond pulsed electric field (ms- μ sPEF)	Liposomes	Small molecule drugs	Improving the transport of nanomedicines	Colon cancer, etc.	Wroclaw Medical University	Phase I/II/III	[246]
	New electrical field ablation	Nanosecond to picosecond pulsed electrical field ablation (ns-psPEF)	Inorganic NPs multi-mode nanomedicine	Small molecule drugs	Improve drug delivery while improving curative effect and preventing recurrence	Liver cancers, etc.	AngioDynamics; Shanghai Ruidao Medical; Hangzhou Ruidi Biotechnology Parade Company; USTB	Preclinical	[247]
Magnetic field (alternating or pulsed am/pmt)		Magnetocaloric (MHT) or magneto-dynamics	Inorganic metal nanoparticles	Iron oxide nanoparticles	High tissue permeability	Nonsmall cell lung cancer, breast cancer	Xiamen University, National University of Singapore	Preclinical	[12]

RF, radiofrequency; CDT: chemodynamic therapy; CLE, chemical luminescent excitation; MRI, magnetic resonance imaging; CT, computed tomography; USTB, University of Science and Technology Beijing (USTB).
Source: Irvine and Dane [47] and Gawne et al. [37].

II [217–224]. (ii) Nanomedicines (e.g. some macromolecule or small molecule nanodrugs encapsulated by polymeric or liposome micelles) mediated traditional EM fields (e.g. RF ablation [RFA]; RF-CDT; microwave ablation [MWT]) can produce RF wave-induced chem-dynamic reaction and/or hyperthermia effects, which can greatly increase the ablation effects and prevent tumor recurrence or metastasis [102, 105]. Both Soochow University; Macau University of Science and Technology, and the fifth medical center of the Chinese People's Liberation Army General Hospital in China have invested in this method, and have paved this combination therapy into the clinical phase I or II in the treatment of breast cancers and the preclinical stage for liver cancers [102, 105]. (iii) There are many new combined therapies developed by new types of nanomedicines mediated new EM field ablation. One of these new therapies is polymeric or metal-based core-shell nanoparticles mediated photoirradiation (photochemical or photodynamics) therapy (PDT), photothermal ablation (PTA), chemiluminescence biochemical reaction excitation (CLE), and pulsed laser photogenesis or photoshock ablation, developed by Fudan Zhangjiang Biopharmaceuticals, AMAG Pharmaceuticals, Advanced Magnetics Inc, Seoul National University, Shanghai Institute of Silicate, Chinese Academy of Sciences, and so on [225–239]. Among them, iron oxide nanomedicines mediated PTA has been in the clinical phase I or II in the treatment of prostate cancer and glioblastoma, showing enhanced curative effects [234, 235]. The second combination is the inorganic or polymeric nanomedicines with sustained luminescence or photosensitivity mediated X-ray radiation for enhanced X-ray photochemical dynamics (PDT) or the radionuclide mediated photochemical dynamic therapy (CR PDT), which can greatly reduce the essential activation dosage of X-ray [240, 241] and/or expand the application scope of X-ray radiation therapy [80, 237]. X-ray radiation-based therapies have been used in the preclinical treatment of breast cancers and/or liver cancers by Memorial Sloan Kettering Cancer Center; Fuzhou University [240, 241] and China Pharmaceutical University [80, 237]. The third combination is the inorganic metal NPs (e.g. Au, Bi, Gd complexes or Cs^{131} like isotope NPs that also preserve MRI, CT, and nuclear resonance multi-mode imaging functions) mediated high energy radiation therapy (HERT: e.g. γ -rays or β -rays emitted by isotopes' decay), which have been in preclinical stage or in the clinical phase I/II stage for the treatment of liver cancer, pancreatic cancer, esophageal cancer, nonsmall cell lung cancer, etc., developed by Johnson&Johnson's subsidiary Janssen Pharmaceuticals, Nanobiotix Company, and Isoray Company [238, 242–245]. (iv) The inorganic NPs, liposome encapsulating small molecules, or inorganic and organic complicated NPs mediated electrical field ablation therapies have been developed from the conventional electrochemical (EDT), ESFP or high-energy millisecond to microsecond PEF (ms- μ sPEF)-based therapies to ultrafast high-energy PEF (ns-psPEF). Among them, nanomedicines mediated ms- μ sPEF therapies have been developed by Wroclaw Medical University entering into the clinical phase I/II/III for the treatment of colon cancers, which can improve the liposome-encapsulating small molecule nanodrugs [246]. Since ns-psPEF ablation therapies have no obvious thermal effect but significant electrical polarization effect, dramatically enhanced cell internalization and lesion

penetration depth of drugs, their combination therapies have been paid much more attention rapidly recently, which have been used in the preclinical study for the treatment of varieties of cancers (e.g. liver cancers) by many company and institutes, such as AngioDynamics in the United States, Shanghai Ruidao Medical Company in China, Hangzhou Ruidi Biotechnology Company in China, Parade Company in China, and University of Science and Technology Beijing in China [207, 247]. (v) The inorganic NPs (e.g. iron oxide NPs) mediated magnetic fields (alternating or pulsed magnetic field) therapies can result in high tissue permeability of drugs due to the magnetocaloric (MHT) or magnetodynamic effects, which have been used in the treatment of nonsmall cell lung cancer and breast cancer by Xiamen University, National University of Singapore and currently in the preclinical stage [12].

Most of these multi-modal therapies by nanomedicines mediated a certain physical field ablation therapy are still in preclinical stages and some of them have been in clinical trials funded by some companies or institutes. Some of them have also shown greatly enhanced immunological effects during their treatment of intractable diseases (e.g. tumors) by comparing with the counterparts of the pure field ablation and/or only nanomedicines. Table 1.3 summarizes ten typical achievements obtained by the main leading institutes or companies in the physical field ablation and/or nanomedicine mediated physical field ablation to date, including types of multi-mode, their therapeutical characteristics and immunological effects, and their current clinical stages. Institutes or companies mainly include Covidien Company [72, 205–207, 217], Massachusetts Institute of Technology [209, 217] and Griffin Adam Holiday Company [88, 210, 211, 217] from the United States; King Saud University from Saudi Arabia [211–214, 216, 251, 252]; Immodulon Therapeutics Ltd. from the United Kingdom [88, 212–215, 217]; Shenzhen Maiwei Medical Company [254, 255], Hangzhou Ruidi Biotechnology Co. Ltd. (HZRD) [256–261], Shanghai Meijie Medical Technology Co. Ltd. [212, 213, 262], USTB and Zhenzhou Tianzhao Biomedical Company [41, 71, 89, 108, 111], and Peking University [268, 269] from China. Types of multi-mode are mostly focusing on the coupling effects from HIFU, electric fields, radiation by varieties of EM waves with broad wavelengths, radiofrequency radiation, temperature gradient induced thermal ablation and nanomedicine enhanced field ablation effects. All these combined therapies based on nanomedicines mediated multi-mode field ablation exhibit significant immunological effects (e.g. inducing inflammatory reactions and promoting the release of tumor antigens to recruit more immune cells and kill cancer cells; activating immune cells and immune regulatory cells; intensifying immune memory; enhancing anti-tumor immune response, and improving expression of related immune factors and immune genes) and the synergistic therapeutical effects (e.g. enhanced ablation effects to kill tumor cells; high penetration depth into lesion and cell internationalization of drugs to enhance the utilization of drugs; intensified dissolution and apoptosis of tumor cells). Particularly, the combined therapies by nanomedicines mediated ns-psPEF developed by USTB and HZRD have shown subversive therapeutic effects using HCC as the pathological model, which can co-stimulate the activation and proliferation of immune cells and promote the inflammatory response and expression of anti-tumor

antigen [41, 89, 108, 123, 207, 270]. Based on the nanomedicine mediated ns-psPEF and high spatiotemporal resolution magneto-optic detection system, Song's group from USTB currently focuses on the development of series of nanomedicine mediated multi-physical-field ablation instruments by coupling rotating or pulsed magnetic fields, laser irradiation and pulsed ultrafast laser, HIFU and ultrafast high intensity PEF [271]. As investigation of the therapeutical effects via multi-physics coupling to nanomedicines using this edge tool, the synergistic immunological effects under different combination modes between multi-physics and multi-mode nanomedicines will be investigated systematically and comprehensively, such as activation of immune cells and immune regulatory cells, enhanced immune memory, reprogram of tumor immune microenvironment, regulation of immune factors and immune gene and their expression-related cytokines and chemokines, as well as the corresponding cell signal and biomolecule pathways.

It can be deduced that the future developed smart nanomedicines with multi-mode imaging, self-targeting transportation and controlled release can not only be used both in visible molecule imaging for the disease precise diagnosis (e.g. tumor classification and phase confirmation) and lesion localization but also their lesion tissue penetration depth and cell internalization can be improved dramatically by the empowerment from the coupling to the corresponding multi-physical fields, leading to smart nanotheranostics [37, 41, 47, 89, 94, 104, 108, 110, 123, 170]. Particularly, for the treatment of cancers, the synergistic effects between the nanomedicines and physical field ablation can endow the corresponding therapy with more flexible intelligent regulation ability on the TIME [127], and consequently, the elimination of cancers and prevention of their recurrence and metastasis will be possibly realized [104, 109, 272, 273].

If readers need more details on the nanomedicines mediated physical field ablation therapy, Chapters 11–15 (“Nanomedicine medicating ultrasound therapy,” “Nanomedicine mediated photodynamic and/or photothermal therapy,” “Nanomedicine mediated pulsed electric field therapy,” “Nanomedicine mediated magneto-dynamic and/or magneto-thermal therapy,” “Nanomedicine mediated radiofrequency or nuclear radiation therapy”) in this monograph can be referred to.

In addition, there are lots of molecule-like features or discrete energy and momentum emerging in some nanomaterials with sizes less than 2 nm (i.e. superatom cluster with atom numbers from one to no more than several hundreds, such as $\text{Au}_{25}\text{L}_{18}$, $\text{Ag}_{44}\text{L}_{30}$, etc., where “L” denotes the ligand, such as thiolate) [274–277]. As they are translated into drugs, they can be called superatom cluster drugs or quantum drugs, which can also include the assemble of these superatom cluster drugs or even some assembly of single atom catalysts of special biological functions (e.g. molecule surgery) [53, 98, 174, 274, 277]. Together with many quantum effects that have also been found in many molecule signal pathways of biological processes (e.g. photosynthesis of chlorophyll) [9, 85, 88, 278]. These superatom cluster drugs will not only promote the progress of nanoenzymes and nanoimmunotherapy but also lead to a new arena in subversive medicines: quantum medicines or quantum drugs (Figure 1.2: one of the major breakthroughs or progresses in 2023) [9, 83–88], for the treatment of many complicated diseases precisely and efficiently, which

Table 1.3 Achievements of multiple physical field ablation and/or multi-mode nanomedicines mediated physical field ablation and the related instrumentation and clinical stages, obtained by 10 currently leading institutes or companies.

Institutes/ Company	Multi-modal therapy via multi-physical field coupling	Typical therapeutical characteristics	Immunological effects	Clinical stage	References
Covidien, United States	High-intensity focused ultrasound, light irradiation/fluorescence excitation	High organizational penetration, spatiotemporal control, synergistic effects, and ROS generation	Promote the release of tumor antigens, activate immune cells, induce inflammatory reactions, and enhance immune memory	Preclinical, Clinical Phase I, II	[204–206, 216, 248]
Massachusetts Inst of Technology, United States	High-intensity focused ultrasound, electric field heating/polarization/perforation/molecular microstructure	High tissue penetration, oxygen independence, and synergistic effects	Dissolution and apoptosis of tumor cells, activation of immune cells, induction of immune memory, and regulation of immune suppression	Preclinical, Clinical Phase I, II	[208, 216, 249]
Griffin Adam Holiday, United States	Light energy irradiation/chemical fluorescence excitation, electric field heating/polarization/perforation/molecular microstructure	Spatiotemporal resolution control, oxygen independence, synergistic effects	Activation and proliferation of immune cells and immune regulatory cells, enhanced anti-tumor immune response, and improved expression of related immune factors	Preclinical	[209, 210, 216, 250]
King Saud University, Saudi Arabia	Nanomagnetic induction hyperthermia; magnetothermal/magnetodynamics; radiotherapy and chemotherapy	Enhancing sensitivity to radiotherapy or chemotherapy	Tissue penetration, targeted therapy, noninvasive, with synergistic effects of nanomedicines	Preclinical, Clinical Phase I, II	[211–214, 216, 251, 252]
Immodulon Therapeutics Ltd., United Kingdom	Low-temperature freezing, radio frequency high-temperature thermal/biochemical reaction activation	High temperature thermal effect, low temperature freezing effect, and cell rupture	Multiple immune cell activation and enhancement, enhanced anti-tumor immune response, and regulation of immune-related gene expression	Preclinical, Clinical Phase I, II	[211–214, 216, 253]

(Continued)

Table 1.3 (Continued)

Institutes/ Company	Multi-modal therapy via multi-physical field coupling	Typical therapeutical characteristics	Immunological effects	Clinical stage	References
Shenzhen Maiwei Medical Company	Low-temperature freezing, pulsed electric field heat- ing/polarization/perforation/ molecular microstructure, RF high-temperature thermal/biochemical reaction activation	Efficient, minimally invasive, precise lesion localization, multi-modal ablation	Antigen release, immune cell activation, inflammatory response, immune memory	Preclinical, clinical phase I, II	[254, 255]
Hangzhou Ruidi Biotechnology Co., Ltd	Low temperature freezing, pulsed electric field heat- ing/polarization/perforation/ molecular microstructure, RF high-temperature thermal/biochemical reaction activation	Efficient, minimally invasive, precise lesion localization, and no heat sink	Stimulation of immune cell activation and proliferation, inflammatory response, regulation of tumor microenvironment, and promotion of tumor antigen expression	Preclinical, Clinical Phase I, II	[256–261]
Shanghai Meijie Medical Technology Co., Ltd	Low temperature freezing, radio frequency high temperature thermal/biochemical reaction activation	Accurate treatment of lesions	Multiple immune cell activation and enhancement, enhanced anti-tumor immune response	Clinical trial	[212, 213, 262]
University of Science and Technology Beijing, Zhenzhou Tianzhao Biomedical Company	Multi-mode nanomedicine mediated ns-psPEF ablation, alternating magnetic field, and laser irradiation; PEF or laser radiation producing ther- mal/polarization/perforation effects; magnetother- mal/magnetodynamics; multi-function activation of nanomedicines	Noninvasive visible targeting lesion at nanoscale; overcoming multi-drug resistance; preventing recurrence and metastasis; regulating tumor cell microenvironment and cytokines; activating immune cells and their proliferation	Nanodrugs coupling multi-field ablation synergistically enhances the activation and the proliferation of immune cells, the inflammatory response, the regulation of tumor microenvironment, and the promotion of tumor antigen expression	Preclinical	[41, 89, 108, 111, 123, 247, 263–267]
Peking University	Light irradiation/fluorescence excitation; magnetother- mal/magnetodynamics; radiotherapy and chemotherapy	Noninvasive, precise treatment of lesions, adjustable treatment effect	Heat stress effect, immune cell activation, inflammatory response, immune memory	Preclinical	[268, 269]

have been paid attention again recently [84, 85, 109, 174, 279]. These quantum medicines may also show great potential in mediating multi-physical field ablation for subversive therapies for intractable diseases.

1.5 Future Development of Nanomedicines by Coupling Advanced Biomedicines (Including Biochemistry and Biophysics), Modern Physicochemical Technologies, and Artificial Intelligence Technology

However, there are still many questions in the development of nanomedicines and the corresponding multi-mode therapies. One of the current key issues is how to obtain these smart nanomedicines with a desired multi-mode imaging function, zymogen-like immune stealth transport ability and special cell or cell microenvironment targeting releasing function. Usually, addressing all of these abilities or functions by one kind of materials is extremely difficult but varieties of materials are coupled together. Fortunately, Song et al. from USTB have developed a novel nanomedicine design strategy as below. The inorganic–organic nanocomposites are constructed based on onion-like nanohybrids of metal alloy or core–shell metal compounds as inorganic cores with multi-mode imaging functions, which can be surface modified and stabilized by organic shells forming inorganic and organic nanocomposites and then conjugating to some organic drugs (e.g. ginsenoside, Paclitaxel, Doxorubicin, antibodies [e.g. PD-L1], etc.) to construct high biocompatible nanomedicine [41, 89, 108]. Finally, these nanomedicines can be encapsulated by hydrogel (e.g. PEG-g-chitosan) or amphiphilic polymers (e.g. PEG-*b*-PLGA) forming nanocapsules or nanovesicles that can be simultaneously surface-linked with some cell or microenvironment specific targeting biomolecules [111]. Recently, Song's group invented a pilot microfluidic process (Figure 1.2) [98], an ultrasonic atomization coupling pyrolysis process, [258, 259, 280] a facile freeze-annealing process [281] and a solid-phase sintering and vapor–liquid–solid growth (SS–VLS-like) method [282] for the large-scale synthesis of these multi-mode nanoparticles, single atom clusters, N, P-doping 3D graphene nanodots supporting quantum dots and as precursors with flexible size (from single atoms to tens of nanometers), shape, composition, and supporter control as well as desired physicochemical properties (e.g. magnetic, optical, electronic, sonic, or mechanical properties) [41, 89, 98, 281, 283–290], for this kind of novel smart nanomedicines or nanoenzymes according to this strategy.

Another key issue is to develop varieties of multi-modal theranostics instruments based on the optimized coupling modes among varieties of nanomedicines and multi-modal ablation determined by varieties of multi-physical-field coupling ablation. Particularly, how to design the key devices or units realizing multi-mode nanomedicines mediated the suitable multi-physical-field coupling ablation instrument with high spatial-temporal resolution (for space time resolution: from μ s to ns or even to fs; for space resolution: from micrometer to nanometer and

even single molecule or ligand level) is crucial to optimize their synergistic effects to develop subversive smart therapies by comprehensively regulating the key immune systems (e.g. immune cells, immunological gene expression, and cell microenvironment) [37, 216, 291, 292]. Overcoming this issue is also essential to fulfill the clinical trials of nanomedicines themselves and these combination therapies [37, 41, 108, 187, 189]. However, this project is not a trivial work. Fortunately, many groups in institutes and companies have been on this road. For example, Song's group in USTB also developed the combined therapy by their multi-mode nanomedicines mediated the nsPEF, which has shown excellent therapeutic effects and great potential in the immune system regulation in the HCC treatment [207]. A novel type of instrument with many subversive features has been on the agenda based on multi-functional nanomedicines mediated multi-physical field coupling ablation by conjugating the rotating or pulsed magnetic fields, laser irradiation and ultrafast pulsed laser, HIFU to their instrument of multi-mode nanomedicines mediated nsPEF ablation [271].

In addition, the recently developed artificial intelligence generation content (AIGC) or machine learning technologies have been successfully used in the rapid and accurate development of varieties of novel specific drugs and therapy designs for intractable diseases [22, 293–296]. AIGC can be further used in the design and microstructure optimization of multi-mode nanomedicines and the assembly of multi-physical fields, as well as the optimization of the coupling modes and key devices, accelerating the instrument development of nanomedicines mediated multi-physical field coupling ablation and the key devices (e.g. tubing type microprobes assembling several physical fields for diagnosis and therapy of diseases). In the following 5–10 years, fundamental research and the key clinical trials of nanomedicines mediated multi-physical field coupling ablation may focus on the following aspects by the combination of progresses in fundamental biomedicines, modern physicochemical technologies, and artificial intelligence: (i) high-throughput design and synthesis methods (e.g. microfluidic processes for drug design and screening) for multi-functional nanohybrids and smart nanomedicines; (ii) basic studies on the interactions between nanomedicines and single cell, sub-cellular units, colossal cells and tissues (particularly for tumor cells and stem cells and neurocytes), the T-cells and B-cells or other immune cells for intractable disease therapy, and the related gene expression and molecular or signal pathway; (iii) nanomedicine database built-up and development assisted by AIGC; (iv) precise and personalized nanomedicine development assisted by AIGC. (v) database building of multi-physical field coupling ablation and their therapeutical effects and immunological effects assisted by AIGC; (vi) subversive therapy development and fundamental biomedical mechanism investigation of nanomedicines mediated multi-physical field ablation assisted by AIGC; and (vii) quantum medicine development for intractable diseases and their therapeutical mechanism study assisted by AIGC. For details on AIGC-assisted design of nanomedicines and combined therapies, readers can refer to Chapters 16 “Nanomedicine conjugating with AI Technology and Genomics for Precise and Personalized Therapy” and 17 “Microfluidic Conjugating AI Platform for High Throughput Nanomedicine Screening” of this monograph.

References

- 1 Xia, C., Dong, X., Li, H. et al. (2022). Cancer statistics in China and United States, 2022: profiles, trends, and determinants. *Chinese Medical Journal* 135: 584–590. <https://doi.org/10.1097/CM9.0000000000002108>.
- 2 Siegel, R.L., Miller, K.D., Wagle, N.S., and Jemal, A. (2023). Cancer statistics, 2023. *CA: A Cancer Journal for Clinicians* 73: 17–48. <https://doi.org/10.3322/caac.21763>.
- 3 <https://www.iarc.fr/faq/latest-global-cancer-data-2020-qa>.
- 4 Nielsen, S.R., Quaranta, V., Linford, A. et al. (2016). Macrophage-secreted granulins supports pancreatic cancer metastasis by inducing liver fibrosis. *Nature Cell Biology* 18: 549–560. <https://doi.org/10.1038/ncb3340>.
- 5 Manfredi, S., Lepage, C., Hatem, C. et al. (2006). Epidemiology and management of liver metastases from colorectal cancer. *Annals of Surgery* 244: 254–259.
- 6 Vidal-Vanaclocha, F. (2008). The prometastatic microenvironment of the liver. *Cancer Microenvironment* 1: 113–129. <https://doi.org/10.1007/s12307-008-0011-6>.
- 7 Kuncic, Z. (2015). Cancer nanomedicine: challenges and opportunities. *The Medical Journal of Australia* 203: 204–205. <https://doi.org/10.5694/mja15.00681>.
- 8 Chen, H., Gu, Z., An, H. et al. (2018). Precise nanomedicine for intelligent therapy of cancer. *Science China. Chemistry* 61: 1503–1552.
- 9 Jain, A., Gosling, J., Liu, S. et al. (2024). Wireless electrical-molecular quantum signalling for cancer cell apoptosis. *Nature Nanotechnology* <https://doi.org/10.1038/s41565-023-01496-y>.
- 10 Yoo, J., Lee, E., Kim, H.Y. et al. (2017). Electromagnetized gold nanoparticles mediate direct lineage reprogramming into induced dopamine neurons in vivo for Parkinson's disease therapy. *Nature Nanotechnology* 12: 1006–1014. <https://doi.org/10.1038/nnano.2017.133>.
- 11 Sun, W., Luo, L., Feng, Y. et al. (2020). Gadolinium–Rose Bengal coordination polymer nanodots for MR-/fluorescence-image-guided radiation and photodynamic therapy. *Advanced Materials* 32: 2000377. <https://doi.org/10.1002/adma.202000377>.
- 12 Zhang, Y., Wang, X., Chu, C. et al. (2020). Genetically engineered magnetic nanocages for cancer magneto-catalytic theranostics. *Nature Communications* 11: 5421. <https://doi.org/10.1038/s41467-020-19061-9>.
- 13 Breton, M. and Mir, L.M. (2012). Microsecond and nanosecond electric pulses in cancer treatments. *Bioelectromagnetics* 33: 106–123. <https://doi.org/10.1002/bem.20692>.
- 14 Ding, X., Stewart, M.P., Sharei, A. et al. (2017). High-throughput nuclear delivery and rapid expression of DNA via mechanical and electrical cell-membrane disruption. *Nature Biomedical Engineering* 1: 0039. <https://doi.org/10.1038/s41551-017-0039>.
- 15 Kotnik, T., Rems, L., Tarek, M., and Miklavčič, D. (2019). Membrane electroporation and electropermeabilization: mechanisms and models. *Annual Review of Biophysics* 48: 63–91. <https://doi.org/10.1146/annurev-biophys-052118-115451>.

- 16 Nuccitelli, R., McDaniel, A., Connolly, R. et al. (2020). Nano-pulse stimulation induces changes in the intracellular organelles in rat liver tumors treated in situ. *Lasers in Surgery and Medicine* 52: 882–889. <https://doi.org/10.1002/lsm.23239>.
- 17 Schoenbach, K.H. and Joshi, R.P. (2010). Bioelectric effects of intense ultrashort pulses. *Critical Reviews in Biomedical Engineering* 38: 255–304. <https://doi.org/10.1615/CritRevBiomedEng.v38.i3.20>.
- 18 Mohamed, N., Lee, A., and Lee, N.Y. (2022). Proton beam radiation therapy treatment for head and neck cancer. *Precision Radiation Oncology* 6: 59–68. <https://doi.org/10.1002/pro6.1135>.
- 19 Matsumoto, Y., Fukumitsu, N., Ishikawa, H. et al. (2021). A critical review of radiation therapy: from particle beam therapy (proton, carbon, and BNCT) to beyond. *Journal of Personalized Medicine* 11: 825. <https://doi.org/10.3390/jpm11080825>.
- 20 Casas, F., Abdel-Wahab, S., Filipovic, N., and Jeremic, B. (2017). *International Encyclopedia of Public Health*, 2nd ed. (ed. S.R. Quah), 260–268. Academic Press.
- 21 Ferreira, T.H. and de Sousa, E.M.B. (2016). *Boron Nitride Nanotubes in Nanomedicine* (ed. G. Ciofani and V. Mattoli), 95–109. William Andrew Publishing.
- 22 Shamay, Y., Shah, J., Işık, M. et al. (2018). Quantitative self-assembly prediction yields targeted nanomedicines. *Nature Materials* 17: 361–368.
- 23 Li, R., He, Y., Zhu, Y. et al. (2019). Route to rheumatoid arthritis by macrophage-derived microvesicle-coated nanoparticles. *Nano Letters* 19: 124–134.
- 24 Furtado, D., Björnmalm, M., Ayton, S. et al. (2018). Overcoming the blood–brain barrier: the role of nanomaterials in treating neurological diseases. *Advanced Materials* 30: 1801362.
- 25 Giardiello, M., Liptrott, N.J., McDonald, T.O. et al. (2016). Accelerated oral nanomedicine discovery from miniaturized screening to clinical production exemplified by paediatric HIV nanotherapies. *Nature Communications* 7: 13184.
- 26 Bourquin, J., Milosevic, A., Hauser, D. et al. (2018). Biodistribution, clearance, and long-term fate of clinically relevant nanomaterials. *Advanced Materials* 30: 1704307.
- 27 Fu, X., Shi, Y., Qi, T. et al. (2020). Precise design strategies of nanomedicine for improving cancer therapeutic efficacy using subcellular targeting. *Signal Transduction and Targeted Therapy* 5: 262. <https://doi.org/10.1038/s41392-020-00342-0>.
- 28 Murray, R.K., Granner, D.K., Mayes, P.A., and Rodwell, V.W. (2003). *Harper's Illustrated Biochemistry*, 26th ed., 693. Lange Medical Books/McGraw-Hill, Medical Publishing Division.
- 29 Glaser, R. (2001). *Biophysics*. 361 pp. Springer-Verlag.
- 30 Bertrand, N., Wu, J., Xu, X. et al. (2014). Cancer nanotechnology: the impact of passive and active targeting in the era of modern cancer biology. *Advanced Drug Delivery Reviews* 66: 2–25. <https://doi.org/10.1016/j.addr.2013.11.009>.
- 31 Greish, K. (2007). Enhanced permeability and retention of macromolecular drugs in solid tumors: a royal gate for targeted anticancer nanomedicines. *Journal of Drug Targeting* 15: 457–464. <https://doi.org/10.1080/10611860701539584>.

- 32 Maeda, H. (2015). Toward a full understanding of the EPR effect in primary and metastatic tumors as well as issues related to its heterogeneity. *Advanced Drug Delivery Reviews* 91: 3–6. <https://doi.org/10.1016/j.addr.2015.01.002>.
- 33 Elnaggar, Y.S.R., Etman, S.M., Abdelmonsif, D.A., and Abdallah, O.Y. (2015). Intranasal piperine-loaded chitosan nanoparticles as brain-targeted therapy in Alzheimer's disease: optimization, biological efficacy, and potential toxicity. *Journal of Pharmaceutical Sciences* 104: 3544–3556.
- 34 Flores, A.M., Hosseini-Nassab, N., Jarr, K.U. et al. (2020). Pro-efferocytic nanoparticles are specifically taken up by lesional macrophages and prevent atherosclerosis. *Nature Nanotechnology* 15: 154–161. <https://doi.org/10.1038/s41565-019-0619-3>.
- 35 Kumar, P., Wu, H., McBride, J.L. et al. (2007). Transvascular delivery of small interfering RNA to the central nervous system. *Nature* 448: 39–43. <https://doi.org/10.1038/nature05901>.
- 36 Yameen, B., Choi, W.I., Vilos, C. et al. (2014). Insight into nanoparticle cellular uptake and intracellular targeting. *Journal of Controlled Release* 190: 485–499. <https://doi.org/10.1016/j.jconrel.2014.06.038>.
- 37 Gawne, P.J., Ferreira, M., Papaluca, M. et al. (2023). New opportunities and old challenges in the clinical translation of nanotheranostics. *Nature Reviews Materials* <https://doi.org/10.1038/s41578-023-00581-x>.
- 38 Kunjachan, S., Ehling, J., Storm, G. et al. (2015). Noninvasive imaging of nanomedicines and nanotheranostics: principles, progress, and prospects. *Chemical Reviews* 115: 10907–10937. <https://doi.org/10.1021/cr500314d>.
- 39 Chen, X., Zhang, X., Guo, Y. et al. (2019). Smart supramolecular “Trojan Horse”-inspired nanogels for realizing light-triggered nuclear drug influx in drug-resistant cancer cells. *Advanced Functional Materials* 29 (13): 1807772. <https://doi.org/10.1002/adfm.201807772>.
- 40 van der Meel, R., Sulheim, E., Shi, Y. et al. (2019). Smart cancer nanomedicine. *Nature Nanotechnology* 14: 1007–1017. <https://doi.org/10.1038/s41565-019-0567-y>.
- 41 Zhao, X., Wu, J., Guo, D. et al. (2022). Dynamic ginsenoside-sheltered nanocatalysts for safe ferroptosis-apoptosis combined therapy. *Acta Biomaterialia* 151: 549–560. <https://doi.org/10.1016/j.actbio.2022.08.026>.
- 42 Xue, X., Huang, Y., Bo, R. et al. (2018). Trojan Horse nanotheranostics with dual transformability and multifunctionality for highly effective cancer treatment. *Nature Communications* 9: 3653. <https://doi.org/10.1038/s41467-018-06093-5>.
- 43 Lee, Y., Kamada, N., and Moon, J.J. (2021). Oral nanomedicine for modulating immunity, intestinal barrier functions, and gut microbiome. *Advanced Drug Delivery Reviews* 179: 114021. <https://doi.org/10.1016/j.addr.2021.114021>.
- 44 He, C., Duan, X., Guo, N. et al. (2016). Core-shell nanoscale coordination polymers combine chemotherapy and photodynamic therapy to potentiate checkpoint blockade cancer immunotherapy. *Nature Communications* 7: 12499. <https://doi.org/10.1038/ncomms12499>.

- 45 Smith, T.T., Stephan, S.B., Moffett, H.F. et al. (2017). In situ programming of leukaemia-specific T cells using synthetic DNA nanocarriers. *Nature Nanotechnology* 12: 813–820. <https://doi.org/10.1038/nnano.2017.57>.
- 46 Yan, G.-H., Wang, K., Shao, Z. et al. (2018). Artificial antibody created by conformational reconstruction of the complementary-determining region on gold nanoparticles. *Proceedings of the National Academy of Sciences* 115: E34. <https://doi.org/10.1073/pnas.1713526115>.
- 47 Irvine, D.J. and Dane, E.L. (2020). Enhancing cancer immunotherapy with nanomedicine. *Nature Reviews Immunology* 20: 321–334. <https://doi.org/10.1038/s41577-019-0269-6>.
- 48 Lakshmanan, V.-K., Jindal, S., Packirisamy, G. et al. (2021). Nanomedicine-based cancer immunotherapy: recent trends and future perspectives. *Cancer Gene Therapy* 28: 911–923. <https://doi.org/10.1038/s41417-021-00299-4>.
- 49 Min, Y., Roche, K.C., Tian, S. et al. (2017). Antigen-capturing nanoparticles improve the abscopal effect and cancer immunotherapy. *Nature Nanotechnology* 12: 877–882. <https://doi.org/10.1038/nnano.2017.113>.
- 50 D’Mello, S.R., Cruz, C.N., Chen, M.L. et al. (2017). The evolving landscape of drug products containing nanomaterials in the United States. *Nature Nanotechnology* <https://doi.org/10.1038/NNANO.2017.67>.
- 51 Conde, J., Oliva, N., Zhang, Y., and Artzi, N. (2016). Local triple-combination therapy results in tumour regression and prevents recurrence in a colon cancer model. *Nature Materials* 15: 1128–1138. <https://doi.org/10.1038/nmat4707>.
- 52 Singha, S., Shao, K., Yang, Y. et al. (2017). Peptide-MHC-based nanomedicines for autoimmunity function as T-cell receptor microclustering devices. *Nature Nanotechnology* 12: 701–710. <https://doi.org/10.1038/nnano.2017.56>.
- 53 Li, Q., Luo, T.Y., Taylor, M.G. et al. (2017). Molecular “surgery” on a 23-gold-atom nanoparticle. *Science Advances* 3: e1603193. <https://doi.org/10.1126/sciadv.1603193>.
- 54 Bai, S., Yang, L.L., Wang, Y. et al. (2020). Prodrug-based versatile nanomedicine for enhancing cancer immunotherapy by increasing immunogenic cell death. *Small* 16: 2000214. <https://doi.org/10.1002/smll.202000214>.
- 55 Cai, J., Wang, H., Wang, D., and Li, Y. (2019). Improving cancer vaccine efficiency by nanomedicine. *Advanced Biosystems* 3: 1800287. <https://doi.org/10.1002/adbi.201800287>.
- 56 Duan, X., He, C., Kron, S.J., and Lin, W. (2016). Nanoparticle formulations of cisplatin for cancer therapy. *Wiley Interdisciplinary Reviews. Nanomedicine and Nanobiotechnology* 8: 776–791. <https://doi.org/10.1002/wnan.1390>.
- 57 Nam, J., Son, S., Park, K.S. et al. (2019). Cancer nanomedicine for combination cancer immunotherapy. *Nature Reviews Materials* 4: 398–414. <https://doi.org/10.1038/s41578-019-0108-1>.
- 58 Zhao, X., Wang, J., Song, Y., and Chen, X. (2018). Synthesis of nanomedicines by nanohybrids conjugating ginsenosides with auto-targeting and enhanced MRI contrast for liver cancer therapy. *Drug Development and Industrial Pharmacy* 44: 1307–1316.

- 59 Bangham, A.D. and Horne, R.W. (1964). Negative staining of phospholipids and their structural modification by surface-active agents as observed in the electron microscope. *Journal of Molecular Biology* 8: 660–668.
- 60 Langer, R. and Folkman, J. (1976). Polymers for the sustained release of proteins and other macromolecules. *Nature* 263: 797–800.
- 61 Matsumura, Y. and Maeda, H. (1986). A new concept for macromolecular therapeutics in cancer chemotherapy: mechanism of tumorotropic accumulation of proteins and the antitumor agent Smancs. *Cancer Research* 46: 6387–6392.
- 62 Gerlowski, L.E. and Jain, R.K. (1986). Microvascular permeability of normal and neoplastic tissues. *Microvascular Research* 31: 288–305.
- 63 Smith, A.D. (2013). Big moment for nanotech: oncology therapeutics poised for a leap. *Oncology Live*® 14 (6) <http://www.onclive.com/publications/Oncology-live/2013/June-2013/Big-Moment-for-Nanotech-Oncology-Therapeutics-Poised-for-a-Leap>.
- 64 US National Library of Medicine. (2013). ClinicalTrials.gov: <https://clinicaltrials.gov/ct2/show/NCT00689065?term>.
- 65 US National Library of Medicine. (2016). *A study of BIND-014 given to patients with advanced or metastatic cancer*. <http://clinicaltrials.gov/ct2/show/NCT01300533?term=NCT01300533&rank=1>.
- 66 Ghadiali, J.E. and Stevens, M.M. (2010). Enzyme-responsive nanoparticle systems. *Advanced Materials* 20: 4359–4363.
- 67 Goto, Y., Yanagi, I., Matsui, K. et al. (2016). Integrated solid-state nanopore platform for nanopore fabrication via dielectric breakdown, DNA-speed deceleration and noise reduction. *Scientific Reports* 6: 31324. <https://doi.org/10.1038/srep31324>.
- 68 Yokoi, K., Kojic, M., Milosevic, M. et al. (2014). Capillary-wall collagen as a biophysical marker of nanotherapeutic permeability into the tumor microenvironment. *Cancer Research* 74: 4239–4246. <https://doi.org/10.1158/0008-5472.Can-13-3494>.
- 69 Yokoi, K., Tanei, T., Godin, B. et al. (2014). Serum biomarkers for personalization of nanotherapeutics-based therapy in different tumor and organ microenvironments. *Cancer Letters* 345: 48–55. <https://doi.org/10.1016/j.canlet.2013.11.015>.
- 70 Folkman, J. and Long, D.M. (1964). The use of silicone rubber as a carrier for prolonged drug therapy. *The Journal of Surgical Research* 4: 139–142.
- 71 Leserman, L.D., Barbet, J., Kourilsky, F., and Weinstein, J.N. (1980). Targeting to cells of fluorescent liposomes covalently coupled with monoclonal antibody or protein A. *Nature* 288: 602–604. <https://doi.org/10.1038/288602a0>.
- 72 Heath, T.D., Fraley, R.T., and Papahdjopoulos, D. (1980). Antibody targeting of liposomes: cell specificity obtained by conjugation of F(ab')₂ to vesicle surface. *Science* 210: 539–541.
- 73 Service, R.F. (2017). Nanoparticles awaken immune cells to fight cancer: in mice, new approach wipes out targeted tumor and metastases as well. *Science News* <https://doi.org/10.1126/science.aal0581>.

- 74 Gref, R., Minamitake, Y., Peracchia, M.T. et al. (1994). Biodegradable long-circulating polymeric nanospheres. *Science* 263: 1600–1603. <https://doi.org/10.1126/science.8128245>.
- 75 Rolland, J.P., Maynor, B.W., Euliss, L.E. et al. (2005). Direct fabrication and harvesting of monodisperse, shape-specific nanobiomaterials. *Journal of the American Chemical Society* 127: 10096–10100.
- 76 Liu, G., Garrett, M.R., Men, P. et al. (2005). Nanoparticle and other metal chelation therapeutics in Alzheimer disease. *Biochimica et Biophysica Acta* 1741: 246–252. <https://doi.org/10.1016/j.bbadis.2005.06.006>.
- 77 Biopharm, S. (2016). *Samyang Biopharm. History*.
- 78 MagForce. (2010). *MagForce. MagForce nanotechnologies AG receives European regulatory approval for its Nano Cancer® therapy*. [magforce.de: http://www.magforce.de/en/presse-investoren/news-events/detail/article/magforce-nanotechnologies-ag-erhaelt-europaeische-zulassung-fuer-die-nano-krebs-therapie.html](http://www.magforce.de/en/presse-investoren/news-events/detail/article/magforce-nanotechnologies-ag-erhaelt-europaeische-zulassung-fuer-die-nano-krebs-therapie.html)
- 79 Hu, C.M.J., Aryal, S., Cheung, C. et al. (2011). Erythrocyte membrane-camouflaged polymeric nanoparticles as a biomimetic delivery platform. *Proceedings of the National Academy of Sciences of the United States of America* 108: 10980–10985.
- 80 Guo, J., Feng, K., Wu, W. et al. (2021). Smart ¹³¹I labeled self-illuminating photosensitizers for deep tumor therapy. *Angewandte Chemie International Edition* 60: 21884–21889.
- 81 Miller, M.A., Gadde, S., Pfirschke, C. et al. (2015). Predicting therapeutic nanomedicine efficacy using a companion magnetic resonance imaging nanoparticle. *Science Translational Medicine* 7: 314ra183. <https://doi.org/10.1126/scitranslmed.aac6522>.
- 82 Sheng, Z., Hu, D., Zheng, M. et al. (2014). Smart human serum albumin-indocyanine green nanoparticles generated by programmed assembly for dual-modal imaging-guided cancer synergistic phototherapy. *ACS Nano* 8: 12310–12322.
- 83 Chi, X., Huang, D., Zhao, Z. et al. (2012). Nanoprobes for in vitro diagnostics of cancer and infectious diseases. *Biomaterials* 33: 189–206. <https://doi.org/10.1016/j.biomaterials.2011.09.032>.
- 84 Wang, Y. and Chen, L. (2011). Quantum dots, lighting up the research and development of nanomedicine. *Nanomedicine: Nanotechnology, Biology, and Medicine* 7: 385–402.
- 85 Bordonaro, M. (2019). Quantum biology and human carcinogenesis. *Biosystems* 178: 16–24. <https://doi.org/10.1016/j.biosystems.2019.01.010>.
- 86 Lambert, N., Chen, Y.N., Cheng, Y.C. et al. (2013). Quantum biology. *Nature Physics* 9: 10–18. <https://doi.org/10.1038/nphys2474>.
- 87 Zingsem, B.W., Feggeler, T., Terwey, A. et al. (2019). Biologically encoded magnonics. *Nature Communications* 10: 4345. <https://doi.org/10.1038/s41467-019-12219-0>.
- 88 Mangalhara, K.C., Varanasi, S.K., Johnson, M.A. et al. (2023). Manipulating mitochondrial electron flow enhances tumor immunogenicity. *Science* 381: 1316–1323. <https://doi.org/10.1126/science.abq1053>.

- 89 Zhang, W., Zhao, X., Yuan, Y. et al. (2020). Microfluidic synthesis of multi-mode Au@CoFeB-Rg3 nanomedicines and their cytotoxicity and anti-tumor effects. *Chemistry of Materials* 32: 5044–5056. <https://doi.org/10.1021/acs.chemmater.0c00797>.
- 90 Wang, W., Mo, W., Hang, Z. et al. (2023). Cuproptosis: harnessing transition metal for cancer therapy. *ACS Nano* 17: 19581–19599. <https://doi.org/10.1021/acsnano.3c07775>.
- 91 Gaetke, L. (2003). Copper toxicity, oxidative stress, and antioxidant nutrients. *Toxicology* 189: 147–163. [https://doi.org/10.1016/s0300-483x\(03\)00159-8](https://doi.org/10.1016/s0300-483x(03)00159-8).
- 92 Liu, Z., Xiong, L., Ouyang, G. et al. (2017). Investigation of copper cysteamine nanoparticles as a new type of radiosensitizers for colorectal carcinoma treatment. *Scientific Reports* 7: 9290.
- 93 Pramanik, A., Pramanik, S., and Pramanik, P. (2017). Copper based nanoparticle: a way towards future cancer therapy. *Global Journal of Nanomedicine* 1: 555573.
- 94 Tsvetkov, P., Coy, S., Petrova, B. et al. (2022). Copper induces cell death by targeting lipoylated TCA cycle proteins. *Science* 375: 1254–1261. <https://doi.org/10.1126/science.abf0529>.
- 95 Yu, Z., Lou, R., Pan, W. et al. (2020). Nanoenzymes in disease diagnosis and therapy. *Chemical Communications* 56: 15513–15524. <https://doi.org/10.1039/D0CC05427E>.
- 96 Liu, J., Zhang, B., Luo, Z. et al. (2015). Enzyme responsive mesoporous silica nanoparticles for targeted tumor therapy in vitro and in vivo. *Nanoscale* 7: 3614–3626.
- 97 The first nano antibody Cabiliv launched after approved by European Marketing Association in Sept 2018 and then by FDA in Feb 2019: <http://vdev.tip-lab.com/article/?uuid=ce20062cc1c44a5396f7eefce6d2a5fb> (2019).
- 98 Wu, Q., Liu, R., Miao, F. et al. (2023). Multimodal ultra-small CoFe-WO_x nanohybrids synthesized by a pilot microfluidic system. *Chemical Engineering Journal* 452: 139355. <https://doi.org/10.1016/j.cej.2022.139355>.
- 99 Nudelman, R., Alhmoud, H., Delalat, B. et al. (2019). Jellyfish-based smart wound dressing devices containing in situ synthesized antibacterial nanoparticles. *Advanced Functional Materials* 29: 1902783. <https://doi.org/10.1002/adfm.201902783>.
- 100 Xu, L., Wang, X., Wang, W. et al. (2022). Enantiomer-dependent immunological response to chiral nanoparticles. *Nature* 601: 366–373. <https://doi.org/10.1038/s41586-021-04243-2>.
- 101 Yang, J. and Zhang, C. (2020). Regulation of cancer-immunity cycle and tumor microenvironment by nanobiomaterials to enhance tumor immunotherapy. *WIREs Nanomedicine and Nanobiotechnology* 12: e1612. <https://doi.org/10.1002/wnan.1612>.
- 102 Hou, Q., Zhang, K., Chen, S. et al. (2022). Physical & chemical microwave ablation (MWA) enabled by nonionic MWA nanosensitizers repress incomplete MWA-arised liver tumor recurrence. *ACS Nano* 16 (4): 5704–5718.

- 103 Li, S., Chen, Z., Tan, L. et al. (2022). MOF@COF nanocapsule for the enhanced microwave thermal-dynamic therapy and anti-angiogenesis of colorectal cancer. *Biomaterials* 283: 121472. <https://doi.org/10.1016/j.biomaterials.2022.121472>.
- 104 Tao, N., Li, H., Deng, L. et al. (2022). A cascade nanozyme with amplified sonodynamic therapeutic effects through comodulation of hypoxia and immunosuppression against cancer. *ACS Nano* 16: 485–501. <https://doi.org/10.1021/acsnano.1c07504>.
- 105 Yang, Z., Zhu, Y., Dong, Z. et al. (2021). Tumor-killing nanoreactors fueled by tumor debris can enhance radiofrequency ablation therapy and boost antitumor immune responses. *Nature Communications* 12: 4299.
- 106 Yin, S., Chen, X., Hu, C. et al. (2014). Nanosecond pulsed electric field (nsPEF) treatment for hepatocellular carcinoma: a novel locoregional ablation decreasing lung metastasis. *Cancer Letters* 346: 285–291.
- 107 Koo, S., Sohn, H.S., Kim, T.H. et al. (2023). Ceria-vesicle nanohybrid therapeutic for modulation of innate and adaptive immunity in a collagen-induced arthritis model. *Nature Nanotechnology* <https://doi.org/10.1038/s41565-023-01523-y>.
- 108 Zhao, X., Wu, J., Zhang, K. et al. (2022). The synthesis of a nanodrug using metal-based nanozymes conjugated with ginsenoside Rg3 for pancreatic cancer therapy. *Nanoscale Advances* 4: 190–199. <https://doi.org/10.1039/D1NA00697E>.
- 109 Zhang, S., Li, Y., Sun, S. et al. (2022). Single-atom nanozymes catalytically surpassing naturally occurring enzymes as sustained stitching for brain trauma. *Nature Communications* 13: 4744. <https://doi.org/10.1038/s41467-022-32411-z>.
- 110 Zou, Y., Jin, B., Li, H. et al. (2022). Cold nanozyme for precise enzymatic anti-tumor immunity. *ACS Nano* 16: 21491–21504. <https://doi.org/10.1021/acsnano.2c10057>.
- 111 Liu, R., Wu, Q., Huang, X. et al. (2021). Synthesis of nanomedicine hydrogel microcapsules by droplet microfluidic process and their pH and temperature dependent release. *RSC Advances* 11: 37814–37823. <https://doi.org/10.1039/D1RA05207A>.
- 112 Miao, Y.-B., Lin, Y.J., Chen, K.H. et al. (2021). Engineering nano- and microparticles as oral delivery vehicles to promote intestinal lymphatic drug transport. *Advanced Materials* 33: 2104139. <https://doi.org/10.1002/adma.202104139>.
- 113 Huang, K.-W., Hsu, F.F., Qiu, J.T. et al. (2020). Highly efficient and tumor-selective nanoparticles for dual-targeted immunogene therapy against cancer. *Science Advances* 6: eaax5032. <https://doi.org/10.1126/sciadv.aax5032>.
- 114 Shi, J., Kantoff, P.W., Wooster, R., and Farokhzad, O.C. (2017). Cancer nanomedicine: progress, challenges and opportunities. *Nature Reviews. Cancer* 17: 20–37. <https://doi.org/10.1038/nrc.2016.108>.
- 115 Roth, T.L., Puig-Saus, C., Yu, R. et al. (2018). Reprogramming human T cell function and specificity with non-viral genome targeting. *Nature* 559: 405–409. <https://doi.org/10.1038/s41586-018-0326-5>.
- 116 Luo, M., Wang, H., Wang, Z. et al. (2017). A STING-activating nanovaccine for cancer immunotherapy. *Nature Nanotechnology* 12: 648–654. <https://doi.org/10.1038/nnano.2017.52>.

- 117 Sengupta, S. (2017). Cancer nanomedicine: lessons for immuno-oncology. *Trends in Cancer* 3: 551–560. <https://doi.org/10.1016/j.trecan.2017.06.006>.
- 118 Yuan, T., Wang, T., Zhang, J. et al. (2023). Robust and multifunctional nanoparticles assembled from natural polyphenols and metformin for efficient spinal cord regeneration. *ACS Nano* 17: 18562–18575. <https://doi.org/10.1021/acsnano.3c06991>.
- 119 Jin, G.R., Mao, D., Cai, P. et al. (2015). Conjugated polymer nanodots as ultra-stable long-term trackers to understand mesenchymal stem cell therapy in skin regeneration. *Advanced Functional Materials* 25: 4263–4273.
- 120 Icli, B., Nabzdyk, C.S., Lujan-Hernandez, J. et al. (2016). Regulation of impaired angiogenesis in diabetic dermal wound healing by microRNA-26a. *Journal of Molecular and Cellular Cardiology* 2016: 151–159.
- 121 Achterberg, V.F., Buscemi, L., Diekmann, H. et al. (2014). The nano-scale mechanical properties of the extracellular matrix regulate dermal fibroblast function. *Journal of Investigative Dermatology* 134: 1862–1872.
- 122 Wu, H., Li, F., Shao, W. et al. (2019). Promoting angiogenesis in oxidative diabetic wound microenvironment using a nanozyme-reinforced self-protecting hydrogel. *ACS Central Science* 5: 477–485. <https://doi.org/10.1021/acscentsci.8b00850>.
- 123 Santos, F.K.D., Oyafuso, M.H., Kiill, C.P. et al. (2013). Nanotechnology-based drug delivery systems for treatment of hyperproliferative skin diseases – a review. *Current Nanoscience* 9: 159–167. <https://doi.org/10.2174/157341313805117857>.
- 124 Long, F., Gu, C., Gu, A.Z., and Shi, H. (2012). Quantum dot/carrier-protein/haptens conjugate as a detection nanobioprobe for FRET-based immunoassay of small analytes with all-fiber microfluidic biosensing platform. *Analytical Chemistry* 84: 3646–3653. <https://doi.org/10.1021/ac3000495>.
- 125 Agrawal, A., Sathe, T., and Nie, S. (2007). *New Frontiers in Ultrasensitive Bioanalysis. Vol. 172 Chemical Analysis: A Series of Monographs on Analysis Chemistry and Its Application* (ed. X.N. Xu), 71–89. John Wiley & Son, Inc.
- 126 Browning, L.M., Lee, K.J., Cherukuri, P.K. et al. (2016). Single nanoparticle plasmonic spectroscopy for study of the efflux function of multidrug ABC membrane transporters of single live cells. *RSC Advances* 6: 36794–36802. <https://doi.org/10.1039/C6RA05895G>.
- 127 Huang, T., Nallathamby, P.D., and Xu, X.-H.N. (2008). Photostable single-molecule nanoparticle optical biosensors for real-time sensing of single cytokine molecules and their binding reactions. *Journal of the American Chemical Society* 130: 17095–17105. <https://doi.org/10.1021/ja8068853>.
- 128 Kyriacou, S.V., Brownlow, W.J., and Xu, X.-H.N. (2004). Using nanoparticle optics assay for direct observation of function of antimicrobial agents in single live bacterial cells. *Biochemistry* 43: 140–147.
- 129 Song, Y., Nallathamby, P.D., Huang, T. et al. (2010). Correlation and characterization of 3D morphological dependent localized surface plasmon resonance spectra of single silver nanoparticles using dark-field optical microscopy and AFM. *Journal of Physical Chemistry C* 114: 74–81.

- 130 Choi, C.K., Li, J., Wei, K. et al. (2015). A gold@polydopamine core-shell nanoprobe for long-term intracellular detection of microRNAs in differentiating stem cells. *Journal of the American Chemical Society* 137: 7337–7346. <https://doi.org/10.1021/jacs.5b01457>.
- 131 Fan, Y. and Zhang, F. (2019). A new generation of NIR-II probes: lanthanide-based nanocrystals for bioimaging and biosensing. *Advanced Optical Materials* 7: 1801417. <https://doi.org/10.1002/adom.201801417>.
- 132 Liu, F., Le, W., Mei, T. et al. (2016). In vitro and in vivo targeting imaging of pancreatic cancer using a $\text{Fe}_3\text{O}_4@\text{SiO}_2$ nanoprobe modified with anti-mesothelin antibody. *International Journal of Nanomedicine* 11: 2195–2207.
- 133 Vo-Dinh, T., Wang, H.-N., and Scaffidi, J. (2009). Plasmonic nanoprobe for SERS biosensing and bioimaging. *Journal of Biophotonics* 3: 89–102.
- 134 Wabuyele, M. and Vo-Dinh, T. (2005). Detection of HIV type 1 DNA sequence using plasmonic nanoprobe. *Analytical Chemistry* 77: 7810–7815.
- 135 Wan, Y., Cheng, G., Liu, X. et al. (2017). Rapid magnetic isolation of extracellular vesicles via lipid-based nanoprobe. *Nature Biomedical Engineering* 1: <https://doi.org/10.1038/s41551-017-0058>.
- 136 Song, Y. (2011). *Recent Advances in Nanofabrication Techniques and Applications*, vol. 1 (ed. B. Cui), 505–532. In-Tech.
- 137 Song, Y. (2009). *Fabrication of high throughput biosensors based on single nanoparticles and nanoparticle arrays*. China patent.
- 138 Pinaud, F., Clarke, S., Sittner, A., and Dahan, M. (2010). Probing cellular events, one quantum dot at a time. *Nature Methods* 7: 275–285. <https://doi.org/10.1038/nmeth.1444>.
- 139 Xu, X.-H.N., Song, Y., and Nallathamby, P. (2007). *New Frontiers in Ultrasensitive Bioanalysis*, vol. 1 (ed. J.D. Winefordner) Ch. 3, 41–70. John Wiley & Son, Inc.
- 140 Letter, T.M. (1973). Griseofulvin: a new formulation and some old concerns. *The Medical Letter on Drugs and Therapeutics* 18: 17–18.
- 141 Rodriguez, P.L., Harada, T., Christian, D.A. et al. (2013). Minimal “self” peptides that inhibit phagocytic clearance and enhance delivery of nanoparticles. *Science* 339: 971–975. <https://doi.org/10.1126/science.1229568>.
- 142 Hajipour, M.J., Laurent, S., Aghaie, A. et al. (2014). Personalized protein coronas: a “key” factor at the nanobiointerface. *Biomaterials Science* 2: 1210–1221.
- 143 Sakulkhu, U., Maurizi, L., Mahmoudi, M. et al. (2014). Ex situ evaluation of the composition of protein corona of intravenously injected superparamagnetic nanoparticles in rats. *Nanoscale* 6: 11439–11450.
- 144 Howard, M., Zern, B.J., Anselmo, A.C. et al. (2014). Vascular targeting of nanocarriers: perplexing aspects of the seemingly straightforward paradigm. *ACS Nano* 8: 4100–4132. <https://doi.org/10.1021/nn500136z>.
- 145 Pridgen, E.M., Alexis, F., Kuo, T.T. et al. (2013). Transepithelial transport of Fc-targeted nanoparticles by the neonatal Fc receptor for oral delivery. *Science Translational Medicine* 5: 213ra167. <https://doi.org/10.1126/scitranslmed.3007049>.

- 146 Cheng, Y., Morshed, R.A., Auffinger, B. et al. (2014). Multifunctional nanoparticles for brain tumor imaging and therapy. *Advanced Drug Delivery Reviews* 66: 42–57. <https://doi.org/10.1016/j.addr.2013.09.006>.
- 147 Xi, Z., Wu, J., Shan, W. et al. (2016). Polymeric nanoparticles amenable to simultaneous installation of exterior targeting and interior therapeutic proteins. *Angewandte Chemie (International Ed. in English)* 55: 3309–3312. <https://doi.org/10.1002/anie.201509183>.
- 148 Samyang Biopharm. (2016). *History*. <https://www.samyangbiopharm.com/eng/Aboutus/history>.
- 149 US National Library of Medicine. (2013). ClinicalTrials.gov, h. c. g. c. s. N. t.
- 150 Espelin, C.W., Leonard, S.C., Geretti, E. et al. (2016). Dual HER2 targeting with trastuzumab and liposomal-encapsulated doxorubicin (MM-302) demonstrates synergistic antitumor activity in breast and gastric cancer. *Cancer Research* 76: 1517–1527.
- 151 Hrkach, J., Von Hoff, D., Ali, M.M. et al. (2012). Preclinical development and clinical translation of a PSMA-targeted docetaxel nanoparticle with a differentiated pharmacological profile. *Science Translational Medicine* 4: 128ra139. <https://doi.org/10.1126/scitranslmed.3003651>.
- 152 Davis, M.E., Zuckerman, J.E., Choi, C.H.J. et al. (2010). Evidence of RNAi in humans from systemically administered siRNA via targeted nanoparticles. *Nature* 464: 1067–1070. <https://doi.org/10.1038/nature08956>.
- 153 Jiang, Y., Krishnan, N., Zhou, J. et al. (2020). Engineered cell-membrane-coated nanoparticles directly present tumor antigens to promote anticancer immunity. *Advanced Materials* 32: 2001808. <https://doi.org/10.1002/adma.202001808>.
- 154 Malhotra, S., Dumoga, S., and Singh, N. (2022). Red blood cells membrane-derived nanoparticles: applications and key challenges in their clinical translation. *Wiley Interdisciplinary Reviews. Nanomedicine and Nanobiotechnology* 14: e1776.
- 155 Dai, Z. (2016). *Advances in Nanotheranostics II*, vol. 551. Springer.
- 156 D'Mello, S.R., Cruz, C.N., Chen, M.L. et al. (2017). The evolving landscape of drug products containing nanomaterials in the United States. *Nature Nanotechnology* 12: 523–530.
- 157 Dixon, S.J., Lemberg, K.M., Lamprecht, M.R. et al. (2012). Ferroptosis: an iron-dependent form of nonapoptotic cell death. *Cell* 149: 1060–1072.
- 158 Liu, T., Liu, W., Zhang, M. et al. (2018). Ferrous-supply-regeneration nanoengineering for cancer-cell-specific ferroptosis in combination with imaging-guided photodynamic therapy. *ACS Nano* 12: 12181–12192.
- 159 Chen, Q., Feng, L., Liu, J. et al. (2016). Intelligent albumin–MnO₂ nanoparticles as pH-/H₂O₂-responsive dissociable nanocarriers to modulate tumor hypoxia for effective combination therapy. *Advanced Materials* 28: 7129–7136. <https://doi.org/10.1002/adma.201601902>.
- 160 Cabral, H., Kinoh, H., and Kataoka, K. (2020). Tumor-targeted nanomedicine for immunotherapy. *Accounts of Chemical Research* 53: 2765–2776. <https://doi.org/10.1021/acs.accounts.0c00518>.

- 161 Dang, Q., Sun, Z., Wang, Y. et al. (2022). Ferroptosis: a double-edged sword mediating immune tolerance of cancer. *Cell Death & Disease* 13: 925. <https://doi.org/10.1038/s41419-022-05384-6>.
- 162 Liu, S., Jiang, Q., Zhao, X. et al. (2020). A DNA nanodevice-based vaccine for cancer immunotherapy. *Nature Materials* <https://doi.org/10.1038/s41563-020-0793-6>.
- 163 Pardi, N., Hogan, M.J., Porter, F.W., and Weissman, D. (2018). mRNA vaccines – a new era in vaccinology. *Nature Reviews Drug Discovery* 17: 261–279. <https://doi.org/10.1038/nrd.2017.243>.
- 164 Pouikli, A. and Frezza, C. (2023). Metabolic control of antitumor immunity. *Science* 381: 1287–1288. <https://doi.org/10.1126/science.adk1785>.
- 165 Ren, Z., Chen, X., Hong, L. et al. (2020). Nanoparticle conjugation of ginsenoside Rg3 inhibits hepatocellular carcinoma development and metastasis. *Small* 16: 1905233. <https://doi.org/10.1002/smll.201905233>.
- 166 Sun, B., Hyun, H., Li, L.-t., and Wang, A.Z. (2020). Harnessing nanomedicine to overcome the immunosuppressive tumor microenvironment. *Acta Pharmacologica Sinica* 41: 970–985. <https://doi.org/10.1038/s41401-020-0424-4>.
- 167 Oliveira, G. and Wu, C.J. (2023). Dynamics and specificities of T cells in cancer immunotherapy. *Nature Reviews Cancer* 23: 295–316. <https://doi.org/10.1038/s41568-023-00560-y>.
- 168 Wadhwa, A., Aljabbari, A., Lokras, A. et al. (2020). Opportunities and challenges in the delivery of mRNA-based vaccines. *Pharmaceutics* 12: 102.
- 169 Yan, W.-l., Lang, T.-q., Yuan, W.-h. et al. (2022). Nanosized drug delivery systems modulate the immunosuppressive microenvironment to improve cancer immunotherapy. *Acta Pharmacologica Sinica* 43: 3045–3054. <https://doi.org/10.1038/s41401-022-00976-6>.
- 170 Cao, F., Sang, Y., Liu, C. et al. (2022). Self-adaptive single-atom catalyst boosting selective ferroptosis in tumor cells. *ACS Nano* 16: 855–868. <https://doi.org/10.1021/acsnano.1c08464>.
- 171 Jiang, X., Stockwell, B.R., and Conrad, M. (2021). Ferroptosis: mechanisms, biology and role in disease. *Nature Reviews Molecular Cell Biology* 22: 266–282. <https://doi.org/10.1038/s41580-020-00324-8>.
- 172 Dale, B., Cheng, M., Park, K.S. et al. (2021). Advancing targeted protein degradation for cancer therapy. *Nature Reviews Cancer* <https://doi.org/10.1038/s41568-021-00365-x>.
- 173 Jiang, D., Ni, D., Rosenkrans, Z.T. et al. (2019). Nanozyme: new horizons for responsive biomedical applications. *Chemical Society Reviews* 48: 3683–3704. <https://doi.org/10.1039/C8CS00718G>.
- 174 Meng, F., Zhu, P., Yang, L. et al. (2023). Nanozymes with atomically dispersed metal centers: structure–activity relationships and biomedical applications. *Chemical Engineering Journal* 452: 139411. <https://doi.org/10.1016/j.cej.2022.139411>.
- 175 Mi, Y., Wolfram, J., Mu, C. et al. (2016). Enzyme-responsive multi-stage vector for drug delivery to tumor tissue. *Pharmacological Research* 113: 92–99.

- 176 Catalano, A., Iacopetta, D., Ceramella, J. et al. (2022). Multidrug resistance (MDR): a widespread phenomenon in pharmacological therapies. *Molecules* 27: 616.
- 177 Tanwar, J., Das, S., Fatima, Z., and Hameed, S. (2014). Multidrug resistance: an emerging crisis. *Interdisciplinary Perspectives on Infectious Diseases* 2014: 541340. <https://doi.org/10.1155/2014/541340>.
- 178 He, C., Poon, C., Chan, C. et al. (2016). Nanoscale coordination polymers code-liver chemotherapeutics and siRNAs to eradicate tumors of cisplatin-resistant ovarian cancer. *Journal of the American Chemical Society* 138: 6010–6019. <https://doi.org/10.1021/jacs.6b02486>.
- 179 Pacios, O., Blasco, L., Bleriot, I. et al. (2020). Strategies to combat multidrug-resistant and persistent infectious diseases. *Antibiotics (Basel)* 9: 65. <https://doi.org/10.3390/antibiotics9020065>.
- 180 Borisov, S.E., d'Ambrosio, L., Centis, R. et al. (2019). Outcomes of patients with drug-resistant-tuberculosis treated with bedaquiline-containing regimens and undergoing adjunctive surgery. *Journal of Infection* 78: 35–39. <https://doi.org/10.1016/j.jinf.2018.08.003>.
- 181 Lammers, T., Sofias, A.M., Van der Meel, R. et al. (2020). Dexamethasone nanomedicines for COVID-19. *Nature Nanotechnology* 15: 622–624. <https://doi.org/10.1038/s41565-020-0752-z>.
- 182 Sun, Q., Bai, X., Sofias, A.M. et al. (2020). Cancer nanomedicine meets immunotherapy: opportunities and challenges. *Acta Pharmacologica Sinica* 41: 954–958. <https://doi.org/10.1038/s41401-020-0448-9>.
- 183 Priem, B., van Leent, M.M., Teunissen, A.J. et al. (2020). Trained immunity-promoting nanobiologic therapy suppresses tumor growth and potentiates checkpoint inhibition. *Cell* 183: 786–801.e719. <https://doi.org/10.1016/j.cell.2020.09.059>.
- 184 Liu, J., Zhang, R., and Xu, Z.P. (2019). Nanoparticle-based nanomedicines to promote cancer immunotherapy: recent advances and future directions. *Small* 15: e1900262. <https://doi.org/10.1002/sml.201900262>.
- 185 Bird, L. (2019). Targeting trained immunity. *Nature Reviews Immunology* 19: 2–3. <https://doi.org/10.1038/s41577-018-0097-0>.
- 186 Mi, Y., Hagan, C.T. IV, Vincent, B.G., and Wang, A.Z. (2019). Emerging nano-/microapproaches for cancer immunotherapy. *Advancement of Science* 6: 1801847.
- 187 Mai, D., June, C.H., and Sheppard, N.C. (2022). In vivo gene immunotherapy for cancer. *Science Translational Medicine* 14: eabo3603. <https://doi.org/10.1126/scitranslmed.abo3603>.
- 188 Allen, G.M., Frankel, N.W., Reddy, N.R. et al. (2022). Synthetic cytokine circuits that drive T cells into immune-excluded tumors. *Science* 378: eaba1624. <https://doi.org/10.1126/science.aba1624>.
- 189 Bear, A.S., Vonderheide, R.H., and O'Hara, M.H. (2020). Challenges and opportunities for pancreatic cancer immunotherapy. *Cancer Cell* 38: 788–802. <https://doi.org/10.1016/j.ccell.2020.08.004>.

- 190 Dobrovolskaia, M.A., Aggarwal, P., Hall, J.B., and McNeil, S.E. (2008). Preclinical studies to understand nanoparticle interaction with the immune system and its potential effects on nanoparticle biodistribution. *Molecular Pharmaceutics* 5: 487–495. <https://doi.org/10.1021/mp800032f>.
- 191 Iwama, R.E. and Moran, Y. (2023). Origins and diversification of animal innate immune responses against viral infections. *Nature Ecology & Evolution* 7: 182–193. <https://doi.org/10.1038/s41559-022-01951-4>.
- 192 Manshian, B.B., Jimenez, J., Himmelreich, U., and Soenen, S.J. (2017). Presence of an immune system increases anti-tumor effect of Ag nanoparticle treated mice. *Advanced Healthcare Materials* 6: 1601099.
- 193 Yang, K., Han, W., Jiang, X. et al. (2022). Zinc cyclic di-AMP nanoparticles target and suppress tumours via endothelial STING activation and tumour-associated macrophage reinvigoration. *Nature Nanotechnology* 17: 1322–1331. <https://doi.org/10.1038/s41565-022-01225-x>.
- 194 Tang, W., Yang, J., Yuan, Y. et al. (2017). Paclitaxel nanoparticle awakens immune system to fight against cancer. *Nanoscale* 9: 6529–6536.
- 195 Garcia, P.A., Ge, Z., Moran, J.L., and Buie, C.R. (2016). Microfluidic screening of electric fields for electroporation. *Scientific Reports* 6: 21238. <https://doi.org/10.1038/srep21238>.
- 196 Weaver, J.C. and Chizmadzhev, Y.A. (1996). Theory of electroporation: a review. *Bioelectrochemistry and Bioenergetics* 41: 135–160. [https://doi.org/10.1016/S0302-4598\(96\)05062-3](https://doi.org/10.1016/S0302-4598(96)05062-3).
- 197 Ni, K., Lan, G., Veroneau, S.S. et al. (2018). Nanoscale metal-organic frameworks for mitochondria-targeted radiotherapy-radiodynamic therapy. *Nature Communications* 9: 4321.
- 198 Jaffee, E.M., Van Dang, C., Agus, D.B. et al. (2017). Future cancer research priorities in the USA: a Lancet Oncology Commission. *The Lancet Oncology* 18: e653–e706. [https://doi.org/10.1016/S1470-2045\(17\)30698-8](https://doi.org/10.1016/S1470-2045(17)30698-8).
- 199 Gu, T., Wang, Y., Lu, Y. et al. (2019). Platinum nanoparticles to enable electrodynamic therapy for effective cancer treatment. *Advanced Materials* 31: 1806803. <https://doi.org/10.1002/adma.201806803>.
- 200 Yang, H., Wang, Q., Li, Z. et al. (2018). Hydrophobicity-adaptive nanogels for programmed anticancer drug delivery. *Nano Letters* 18: 7909–7918.
- 201 Adir, O., Poley, M., Chen, G. et al. (2020). Integrating artificial intelligence and nanotechnology for precision cancer medicine. *Advanced Materials* 32: 1901989. <https://doi.org/10.1002/adma.201901989>.
- 202 Yang, B. and Shi, J. Chemistry of advanced nanomedicines in cancer cell metabolism regulation. *Advanced Science* 32: 2001388. <https://doi.org/10.1002/advs.202001388>.
- 203 Ho, D., Wang, P., and Kee, T. (2019). Artificial intelligence in nanomedicine. *Nanoscale Horizons* 4: 365–377. <https://doi.org/10.1039/C8NH00233A>.
- 204 堵建岗 & 激光生物学报 (2015). 劳. J. 光动力学结合声动力学治疗对小鼠鳞癌细胞超微结构的影响. 33-36+65.
- 205 李维娜 et al. (2010). 光动力学疗法和声动力学疗法. 27, 5.

- 206 Li, J.-H., Chen, Z.-Q., Huang, Z. et al. (2013). In vitro study of low intensity ultrasound combined with different doses of PDT: effects on C₆ glioma cells. *Oncology Letters* 5: 702–706.
- 207 赵梹雄 (2022). 多模铁基纳米药物联合纳秒脉冲抗肿瘤疗效及其机制研究 博士学位, 北京科技大学.
- 208 电场和超声波结合治疗癌症 %J 上海生物医学工程. 26, 1 (2005).
- 209 Melo, W.d.C.M.A.d., Celieiūt-Germanien, R., Imonis, P., and Virulence, A.S.J. (2021). Antimicrobial photodynamic therapy (aPDT) for biofilm treatments. Possible synergy between aPDT and pulsed electric fields. *Virulence* 12: 2247–2272.
- 210 de Cássia Martins Antunes Melo, W., Lee, A.N., Perussi, J.R., and Hamblin, M.R. (2013). Electroporation enhances antimicrobial photodynamic therapy mediated by the hydrophobic photosensitizer, hypericin. *Photodiagnosis and Photodynamic Therapy* 10: 647–650.
- 211 德国磁感应研究取得突破性进展 (2003). <http://muchong.com/html/201108/3451682.html>.
- 212 癌症治疗大势所趋!新型多模态冷冻消融技术+靶向治疗! (2020). <https://www.innomd.org/article/5f6d53b0218ba11792991907>.
- 213 “冷热” 兼攻, “交复” 联手, 全球首发多模态肿瘤治疗系统, 迎来抗癌新时代 (2023). <https://new.qq.com/rain/a/20230715A06IMB00>.
- 214 「初创」 顶尖的医疗器械初创企业系列(四) (2023). <https://baijiahao.baidu.com/s?id=175079263383377119&wfr=spider&for=pc>.
- 215 Wenjun, X., Xie, X., Wu, H. et al. (2022). Pulsed electromagnetic therapy in cancer treatment: progress and outlook. *Wiley Online Library* 3: 11–12.
- 216 赵梹雄 (2022). 多模铁基纳米药物联合纳秒脉冲抗肿瘤疗效及其机制研究, 北京科技大学.
- 217 Son, S., Kim, J., Kim, J. et al. (2022). Cancer therapeutics based on diverse energy sources. *Chemical Society Reviews* 51: 8201–8215. <https://doi.org/10.1039/D2CS00102K>.
- 218 Dimceviski, G., Kotopoulis, S., Bjånes, T. et al. (2016). A human clinical trial using ultrasound and microbubbles to enhance gemcitabine treatment of inoperable pancreatic cancer. *Journal of Controlled Release* 243: 172–181.
- 219 Duan, L., Yang, L., Jin, J. et al. (2020). Micro/nano-bubble-assisted ultrasound to enhance the EPR effect and potential theranostic applications. *Theranostics* 10: 462–483.
- 220 Morse, S.V., Mishra, A., Chan, T.G. et al. (2022). Liposome delivery to the brain with rapid short-pulses of focused ultrasound and microbubbles. *Journal of Controlled Release* 341: 605–615.
- 221 Morse, S.V., Pouliopoulos, A.N., Chan, T.G. et al. (2019). Rapid short-pulse ultrasound delivers drugs uniformly across the murine blood–brain barrier with negligible disruption. *Radiology* 291: 459–466.
- 222 Theek, B., Baues, M., Ojha, T. et al. (2016). Sonoporation enhances liposome accumulation and penetration in tumors with low EPR. *Journal of Controlled Release* 231: 77–85.
- 223 Centelles, M.N., Wright, M., So, P.W. et al. (2018). Image guided thermosensitive liposomes for focused ultrasound drug delivery: using NIRF labelled lipids

- and topotecan to visualise the effects of hyperthermia in tumours. *Journal of Controlled Release* 280: 87–98.
- 224 Fan, Z., Wang, Y., Li, L. et al. (2022). Tumor-homing and immune-reprogramming cellular nanovesicles for photoacoustic imaging-guided phototriggered precise chemoimmunotherapy. *ACS Nano* 16: 16177–16190.
 - 225 Thebault, C.J., Ramniceanu, G., Boumati, S. et al. (2020). Theranostic MRI liposomes for magnetic targeting and ultrasound triggered release of the anti-vascular CA₄P. *Journal of Controlled Release* 322: 137–148. <https://doi.org/10.1016/j.jconrel.2020.03.003>.
 - 226 Chen, L.J., Yang, C.X., and Yan, X.P.J.A.C. (2017). Liposome-coated persistent luminescence nanoparticles as luminescence trackable drug carrier for chemotherapy. *Analytical Chemistry* 89: 6936–6939.
 - 227 Liu, J., He, S., Luo, Y. et al. (2022). Tumor-microenvironment-activatable polymer nano-immunomodulator for precision cancer photoimmunotherapy. *Advanced Materials* 34: e2106654. <https://doi.org/10.1002/adma.202106654>.
 - 228 Lu, Y., Song, G., He, B. et al. (2020). Strengthened tumor photodynamic therapy based on a visible nanoscale covalent organic polymer engineered by microwave assisted synthesis. *Advanced Functional Materials* 30: 2004834. <https://doi.org/10.1002/adfm.202004834>.
 - 229 Maldiney, T., Bessière, A., Seguin, J. et al. (2014). The in vivo activation of persistent nanophosphors for optical imaging of vascularization, tumours and grafted cells. *Nature Materials* 13: 418–426. <https://doi.org/10.1038/nmat3908>.
 - 230 Wang, J., Ma, Q., Hu, X.X. et al. (2017). Autofluorescence-free targeted tumor imaging based on luminous nanoparticles with composition-dependent size and persistent luminescence. *ACS Nano* 11: 8010–8017.
 - 231 Zheng, B., Bai, Y., Chen, H. et al. (2018). Near-infrared light-excited upconverting persistent nanophosphors in vivo for imaging-guided cell therapy. *ACS Applied Materials & Interfaces* 10: 19514–19522. <https://doi.org/10.1021/acsami.8b05706>.
 - 232 Cho, M., Cervadoro, A., Ramirez, M.R. et al. (2017). Assembly of iron oxide nanocubes for enhanced cancer hyperthermia and magnetic resonance imaging. *Nanomaterials (Basel)* 7: 72.
 - 233 Du, Y., Liu, X., Liang, Q. et al. (2019). Optimization and design of magnetic ferrite nanoparticles with uniform tumor distribution for highly sensitive MRI/MPI performance and improved magnetic hyperthermia therapy. *Nano Letters* 19: 3618–3626.
 - 234 Hirsch, L.R., Stafford, R.J., Bankson, J.A. et al. (2003). Nanoshell-mediated near-infrared thermal therapy of tumors under magnetic resonance guidance. *Proceedings of the National Academy of Sciences of the United States of America* 100: 13549–13554.
 - 235 Mai, B.T., Balakrishnan, P.B., Barthel, M.J. et al. (2019). Thermoresponsive iron oxide nanocubes for an effective clinical translation of magnetic hyperthermia and heat-mediated chemotherapy. *ACS Applied Materials & Interfaces* 11: 5727–5739.

- 236 Maier-Hauff, K., Ulrich, F., Nestler, D. et al. (2011). Efficacy and safety of intra-tumoral thermotherapy using magnetic iron-oxide nanoparticles combined with external beam radiotherapy on patients with recurrent glioblastoma multiforme. *Journal of Neuro-Oncology* 103: 317–324.
- 237 Rastinehad, A.R., Anastos, H., Wajswol, E. et al. (2019). Gold nanoshell-localized photothermal ablation of prostate tumors in a clinical pilot device study. *Proceedings of the National Academy of Sciences of the United States of America* 116: 18590–18596.
- 238 Lee, W., Jeon, M., Choi, J. et al. (2020). Europium-diethylenetriaminepentaacetic acid loaded radioluminescence liposome nanoplatform for effective radioisotope-mediated photodynamic therapy. *ACS Nano* 14: 13004–13015. <https://doi.org/10.1021/acsnano.0c04324>.
- 239 Liu, Y., Liu, Y., Bu, W. et al. (2015). Hypoxia induced by upconversion-based photodynamic therapy: towards highly effective synergistic bioreductive therapy in tumors. *Angewandte Chemie, International Edition* 54: 8105–8109. <https://doi.org/10.1002/anie.201500478>.
- 240 Yu, Z., Zhou, P., Pan, W. et al. (2018). A biomimetic nanoreactor for synergistic chemiexcited photodynamic therapy and starvation therapy against tumor metastasis. *Nature Communications* 9: 1–9.
- 241 Larson, S.M., Carrasquillo, J.A., Cheung, N.K.V., and Press, O.W. (2015). Radioimmunotherapy of human tumours. *Nature Reviews Cancer* 15: 509–509.
- 242 Song, L., Li, P.P., Yang, W. et al. (2018). Low-dose X-ray activation of W(VI)-doped persistent luminescence nanoparticles for deep-tissue photodynamic therapy. *Advanced Functional Materials* 28: 1707496.
- 243 Bort, G., Lux, F., Dufort, S. et al. (2020). EPR-mediated tumor targeting using ultrasmall-hybrid nanoparticles: from animal to human with theranostic AGuIX nanoparticles. *Theranostics* 10: 1319–1331.
- 244 Ma, M., Huang, Y., Chen, H. et al. (2015). Bi₂S₃-embedded mesoporous silica nanoparticles for efficient drug delivery and interstitial radiotherapy sensitization. *Biomaterials* 37: 447–455.
- 245 Marill, J., Anesary, N.M., Zhang, P. et al. (2014). Hafnium oxide nanoparticles: toward an in vitro predictive biological effect? *Radiation Oncology* 9: <https://doi.org/10.1186/1748-717x-9-150>.
- 246 IsoRay. <http://www.maydeal.com/news/7829.html>.
- 247 Kulbacka, J., Pucek, A., Wilk, K.A. et al. (2016). The effect of millisecond pulsed electric fields (msPEF) on intracellular drug transport with negatively charged large nanocarriers made of solid lipid nanoparticles (SLN): in vitro study. *The Journal of Membrane Biology* 249: 645–661.
- 248 Thiesen, B. and Jordan, A. (2008). Clinical applications of magnetic nanoparticles for hyperthermia. *International Journal of Hyperthermia* 24: 467–474. <https://doi.org/10.1080/02656730802104757>.
- 249 Faruq Mohammad, A. and Al-Lohedan, H.A. (2020). Multifunctional cancer targeting nanoparticles. US10561747B1.
- 250 【首发】布局行业领先的多模态能量平台产品,迈微医疗完成数千万元 Pre-A 轮融资 (2023). http://news.sohu.com/a/650021191_133140.

- 251 Shenzhen Maiwei Medical Technology Co, L. (2022). *L. ablation catheter and multimodal ablation equipment*. Chinese invention patent, approval number: CN217907970U.
- 252 睿笛生物:以全球领先的纳秒脉冲电场技术,突破肿瘤消融禁区,布局心血管疾病 (2021). https://www.sohu.com/a/484907888_133140.
- 253 陈新华 & 等. 国家科技重大专项“原始创新型纳秒刀精准消融肝癌抗复发转移的研发及临床应用研究:项目编号:2018ZX10301201”结题报告 (2021).
- 254 Chen Yonggang (2021). *An adaptive pulse ablation instrument based on electrocardiogram waveform*. Chinese invention patent, approval number: ZL201910247941.8.
- 255 Chen Yonggang (2021). *A ablation electrode positioning system*. Chinese invention patent, approval number: ZL201811023704.5.
- 256 Yonggang, C. (2021). *A closed-loop control system for pulse ablation*. China invention patent, issued number: ZL202111466101.4.
- 257 Yonggang, C. (2022). *A miniaturized nanosecond pulse generation system for tumor ablation*. China Invention Patent Issued number: ZL202111495485.2.
- 258 Shanghai Meijie Medical Technology Co., L. (2023). *Multimodal tumor ablation probe system and its control method*. China patent.
- 259 Wang, Z., Zhang, F., Shao, D. et al. (2019). Janus nanobullets combine photodynamic therapy and magnetic hyperthermia to potentiate synergetic anti-metastatic immunotherapy. *Advanced Science (Weinh)* 6: 1901690.
- 260 University, P (2020). *Superconducting rotating frame for laser accelerated proton cancer treatment device*. Chinese invention patent, approval number: CN111790063A.
- 261 Yang, X., Wu, Q., Zhao, X. et al. (2023). Pulsed electric field technology translational medicine. *Small* submitted.
- 262 Song, Y. and Yang, X. (2023). *An instrument for the nanomedicine mediating multi-physics coupling ablation*. China patent.
- 263 *Autonomous ultrasound guided endoscope*. USA patent (2022).
- 264 MIT. (2000). *Effect of electric field and ultrasound for transdermal drug delivery*.
- 265 Holiday, G. A. (2012). *Pulsed power laser actuated catheter system for interventional oncology*. US Patent, approval number: US2012165808A1.
- 266 LTD, I. T (2013). *Immunogenic treatment of cancer*. Application number: WO2013079980A1.
- 267 宋玉军 and 等. 国家科技重大专项“原始创新型纳秒刀精准消融肝癌抗复发转移的研发及临床应用研究: 项目编号:2018ZX10301201“课题四”纳秒脉冲联合纳米药物精准消融肝癌及其机制研究“结题报告. (2021).
- 268 Yujun, S. (2009). *Preparation process of single nanoparticle and its array based biomolecular detectors*. China Invention Patent Issued number: ZL 200910085973.9.
- 269 Wenqi, S., Yujun, S., and Wang, J (2015). *A anticancer alloy nanodrug with autonomous targeting and imaging functions and its preparation method*. China Invention Patent Issued number: ZL 201510395518.4.
- 270 Yujun, S. (2018). *Construction of composite nanomedicine by coupling drug components with nanoparticles, preparation method and application*.

- 271 Yujun, S. and Jugang, M. (2020). *A device and method for large-scale continuous preparation of metal nanoparticles*. Chinese invention patent approval number: ZL 2020 11462174.1.
- 272 Ohki, Y., Munakata, K., Matsuoka, Y. et al. (2022). Nitrogen reduction by the Fe sites of synthetic $[\text{Mo}_3\text{S}_4\text{Fe}]$ cubes. *Nature* 607: 86–90. <https://doi.org/10.1038/s41586-022-04848-1>.
- 273 Li, X., Khorsandi, S., Wang, Y. et al. (2022). Cancer immunotherapy based on image-guided STING activation by nucleotide nanocomplex-decorated ultrasound microbubbles. *Nature Nanotechnology* 17: 891–899. <https://doi.org/10.1038/s41565-022-01134-z>.
- 274 Mathew, A. and Pradeep, T. (2014). Noble metal clusters: applications in energy, environment, and biology. *Particle & Particle Systems Characterization* 31: 1017–1053. <https://doi.org/10.1002/ppsc.201400033>.
- 275 Chakraborty, P., Nag, A., Chakraborty, A., and Pradeep, T. (2019). Approaching materials with atomic precision using supramolecular cluster assemblies. *Accounts of Chemical Research* 52: 2–11. <https://doi.org/10.1021/acs.accounts.8b00369>.
- 276 Jena, P. and Sun, Q. (2018). Super atomic clusters: design rules and potential for building blocks of materials. *Chemical Reviews* 118: 5755–5870. <https://doi.org/10.1021/acs.chemrev.7b00524>.
- 277 Jena, P. (2022). Superatomic chemistry. *Journal of the Indian Chemical Society* 99: 100350. <https://doi.org/10.1016/j.jics.2022.100350>.
- 278 Devault, D., Parkes, J.H., and Chance, B. (1967). Electron tunnelling in cytochromes. *Nature* 215: 642–644.
- 279 O'Brien, E., Holt, M.E., Thompson, M.K. et al. (2017). The $[\text{4Fe4S}]$ cluster of human DNA primase functions as a redox switch using DNA charge transport. *Science* 355: eaag1789. <https://doi.org/10.1126/science.aag1789>.
- 280 Wang, Y., Liu, R., Chen, T. et al. (2024). $\text{CoFe}@\text{[CoFe}_2\text{O}_4\text{/Fe(Co)Nx-C]}$ nanoparticles prepared via an ultrasonic atomization coupling pyrolysis process and their magnetic and optical properties. *Journal of Alloys and Compounds* 970: 172358. <https://doi.org/10.1016/j.jallcom.2023.172358>.
- 281 Tong, X., Linong, L., Xiaona, Y. et al. (2021). N,P-codoped graphene dots supported on N-doped 3D graphene as metal-free catalysts for oxygen reduction. *ACS Applied Materials & Interfaces* 13: 30512–30523. <https://doi.org/10.1021/acsami.1c03141>.
- 282 Liao, Q., Hou, W., Liao, K. et al. (2022). Solid-phase sintering and vapor-liquid-solid growth of BP@MgO quantum dot crystals with a high piezoelectric response. *Journal of Advanced Ceramics* 11: 1725–1734. <https://doi.org/10.1007/s40145-022-0643-x>.
- 283 Ma, J., Tong, X., Wang, J. et al. (2019). Rare-earth metal oxide hybridized PtFe nanocrystals synthesized via microfluidic process for enhanced electrochemical catalytic performance. *Electrochimica Acta* 299: 80–88. <https://doi.org/10.1016/j.electacta.2018.12.132>.

- 284 Ma, J., Wang, L., Deng, Y. et al. (2021). Mass production of high performance single atomic FeNC electrocatalysts via a sequenced ultrasonic atomization, pyrolysis. *Science China Materials* 64: 631–641.
- 285 Ma, J., Wu, Q., Zhang, W. et al. (2022). Synergetic contribution of $\text{Co}^{3+}/\text{Co}^{2+}$ and FeNC in $\text{CoFe@CoFe}_2\text{O}_4$ toward efficient electrocatalysts for oxygen reduction reaction. *Electrochimica Acta* 432: 141224. <https://doi.org/10.1016/j.electacta.2022.141224>.
- 286 Liang, H., Wang, Z., Junmei, W. et al. Synthesis of $\text{Fe}_{(1-x)}\text{Zn}_x@\text{Zn}_{(1-y)}\text{Fe}_y\text{O}_z$ nanocrystals via a simple programmed microfluidic process. *Materials Chemistry and Physics* 201: 156–164.
- 287 Wang, J., Wang, Z., Li, S. et al. (2017). Surface and interface engineering of FePt/C nanocatalysts for electro-catalytic methanol oxidation: enhanced activity and durability. *Nanoscale* 9: 4037–4312. <https://doi.org/10.1039/c6nr09122a>.
- 288 Wang, J., Zhao, H., Zhu, Y., and Song, Y. (2017). Shape-controlled synthesis of CdSe nanocrystals via a programmed microfluidic process. *Journal of Physical Chemistry C* 121: 3567–3572. <https://doi.org/10.1021/acs.jpcc.6b10901>.
- 289 Wang, R., Yang, W., Song, Y. et al. (2015). A general strategy for nanohybrids synthesis via coupled competitive reactions controlled in a hybrid process. *Scientific Reports* 5: 9189.
- 290 Zhao, X., Liang, H., Chen, Y. et al. (2021). Magnetic field coupling microfluidic synthesis of diluted magnetic semiconductor quantum dots: the case of Co doping ZnSe quantum dots. *Journal of Materials Chemistry C* 9: 4619–4627. <https://doi.org/10.1039/D0TC06026G>.
- 291 Huang, L., Li, Y., Du, Y. et al. (2019). Mild photothermal therapy potentiates anti-PD-L1 treatment for immunologically cold tumors via an all-in-one and all-in-control strategy. *Nature Communications* 10: 4871. <https://doi.org/10.1038/s41467-019-12771-9>.
- 292 Shi, L., Wang, J., Ding, N. et al. (2019). Inflammation induced by incomplete radiofrequency ablation accelerates tumor progression and hinders PD-1 immunotherapy. *Nature Communications* 10: 5421. <https://doi.org/10.1038/s41467-019-13204-3>.
- 293 Jumper, J., Evans, R., Pritzel, A. et al. (2021). Highly accurate protein structure prediction with AlphaFold. *Nature* 596: 583–589. <https://doi.org/10.1038/s41586-021-03819-2>.
- 294 Fan, K., Cheng, L., and Li, L. (2021). Artificial intelligence and machine learning methods in predicting anti-cancer drug combination effects. *Briefings in Bioinformatics* 22: <https://doi.org/10.1093/bib/bbab271>.
- 295 Decherchi, S., Berteotti, A., Bottegoni, G. et al. (2015). The ligand binding mechanism to purine nucleoside phosphorylase elucidated via molecular dynamics and machine learning. *Nature Communications* 6: 6155. <https://doi.org/10.1038/ncomms7155>.
- 296 Stokes, J.M., Yang, K., Swanson, K. et al. (2020). A deep learning approach to antibiotic discovery. *Cell* 180: 688–702.e613. <https://doi.org/10.1016/j.cell.2020.01.021>.